

## Research paper

## Calcium buffers and L-type calcium channels as modulators of cardiac subcellular alternans



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## ABSTRACT

In cardiac myocytes, calcium cycling links the dynamics of the membrane potential to the activation of the contractile filaments. Perturbations of the calcium signalling toolkit have been demonstrated to disrupt this connection and lead to numerous pathologies including cardiac alternans. This rhythm disturbance is characterised by alternations in the membrane potential and the intracellular calcium concentration, which in turn can lead to sudden cardiac death. In the present computational study, we make further inroads into understanding this severe condition by investigating the impact of calcium buffers and L-type calcium channels on the formation of subcellular calcium alternans when calcium diffusion in the cytosol is weak and the main route of  $\text{Ca}^{2+}$  transport in the myocyte is via the sarcoplasmic reticulum. Through numerical simulations of a two dimensional network of calcium release units, we show that increasing calcium entry is proarrhythmogenic and that this is modulated by the calcium-dependent inactivation of the L-type calcium channel. We also find that while calcium buffers can exert a stabilising force and abolish subcellular  $\text{Ca}^{2+}$  alternans, they can significantly shape the spatial patterning of subcellular calcium alternans. Taken together, our results demonstrate that subcellular calcium alternans can emerge via various routes and that calcium diffusion in the sarcoplasmic reticulum critically determines their spatial patterns.

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## 1. Introduction

Cardiac arrhythmias constitute a leading public health problem and cause most cases of sudden cardiac death. In the US alone, sudden cardiac death accounts for approximately 300,000–450,000 lives every year [1]. Among the many forms of cardiac arrhythmias, cardiac alternans feature prominently. This rhythm disturbance at the level of a single cardiac myocyte is characterised by alternating patterns of the membrane potential and the intracellular calcium ( $\text{Ca}^{2+}$ ) concentration on successive beats. For instance, at one beat, a long action potential duration (APD) is accompanied by a large intracellular  $\text{Ca}^{2+}$  transient, while on the next beat, the APD is shortened concomitant with a small amplitude  $\text{Ca}^{2+}$  transient. As a consequence, contractile efficiency is impaired, which in turn can cause a detrimental reduction in blood flow. In early experimental studies, the intracellular  $\text{Ca}^{2+}$  concentration was averaged across a cardiac myocyte. The advent of high-resolution microscopy revealed that alternating  $\text{Ca}^{2+}$  dynamics were already present at individual  $\text{Ca}^{2+}$  release units (CRU)

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[2–4]. While one CRU follows a pattern of large-small-large  $\text{Ca}^{2+}$  transients, neighbouring CRUs exhibit small-large-small  $\text{Ca}^{2+}$  transients. Crucially, both CRUs experience the same membrane potential. These findings gave rise to the concept of subcellular  $\text{Ca}^{2+}$  alternans [5–13] and illustrated that nonlinear processes govern cardiac dynamics across multiple scales: the cell wide membrane potential and the  $\text{Ca}^{2+}$  fluxes restricted to single dyadic clefts.

The existence of subcellular  $\text{Ca}^{2+}$  alternans reinforces the notion of cardiac myocytes as a network of networks. Each CRU can be conceptualised as a network of interacting components such as L-type  $\text{Ca}^{2+}$  channels, sodium-calcium exchangers (NCXs) and ryanodine receptors (RyRs). These local networks are then coupled via  $\text{Ca}^{2+}$  diffusion through both the cytosol and the sarcoplasmic reticulum (SR). This interconnectedness offers multiple explanations for the origin of subcellular  $\text{Ca}^{2+}$  alternans. On the one hand, we have previously shown [14] that  $\text{Ca}^{2+}$  alternans can emerge purely through coupling. In [14], we initially considered a coupled CRU network in which each node exhibited a regular period-1 orbit, i.e. the network mimicked a physiologically healthy state. Upon increasing the coupling strength between the nodes, i.e. decreasing  $\tau_c$  in Eq. (1b), and *without* changing any other parameter values, we observed alternating solutions in which neighbouring CRUs oscillated out-of-phase. A key step in this study was the derivation of a map  $\Gamma$  that linked an initial perturbation of the CRU network  $\delta y_0$  around the synchronous network state (which corresponds to the physiologically healthy state of the myocyte) to its final state  $\delta y_f$  after one pacing period:  $\delta y_f = \Gamma \delta y_0$ . We found that one eigenvalue of the matrix  $\Gamma$  exited the unit disk through  $-1$  along the real axis upon decreasing  $\tau_c$ , which is consistent with the subcellular  $\text{Ca}^{2+}$  alternans that we observed in direct numerical simulations of the CRU network. Crucially, the spatial patterns of the subcellular  $\text{Ca}^{2+}$  alternans may depend on whether  $\text{Ca}^{2+}$  diffusion is stronger in the cytosol or in the SR. In a recent model of  $\text{Ca}^{2+}$  cycling [15,16],  $\text{Ca}^{2+}$  alternans emerge for dominant cytosolic coupling via the traditional period-doubling bifurcation, where an eigenvalue of  $\Gamma$  leaves the unit disk at  $-1$  along the real line. In addition to the findings in [14], we also observed subcellular  $\text{Ca}^{2+}$  alternans where different parts of the cell oscillate out-of-phase as seen experimentally in e.g. [8]. However, for dominant luminal coupling, there is a saddle-node bifurcation of the map  $\Gamma$ , where the leading eigenvalue leaves the unit disk at  $+1$  along the real axis. In this case, each node follows a period-1 orbit, but the amplitudes of neighbouring CRUs varies. On the other hand, changes to the molecular components of a CRU can induce  $\text{Ca}^{2+}$  alternans, exemplified by weakening sarco-endoplasmic  $\text{Ca}^{2+}$  ATP (SERCA) pumps or increasing  $\text{Ca}^{2+}$  flux through L-type  $\text{Ca}^{2+}$  channels.

To date, investigations on how  $\text{Ca}^{2+}$  alternans emerge due to modifications at the CRU level have almost exclusively focussed on dominant cytosolic coupling [6,17–23]. However, the question as to whether  $\text{Ca}^{2+}$  diffusion in the SR is slow or fast – and hence weak or strong – is still unanswered [24–26]. Here, we focus on stronger SR  $\text{Ca}^{2+}$  diffusion in the presence of weak cytosolic  $\text{Ca}^{2+}$  diffusion and explore the impact of two modifiers of the local  $\text{Ca}^{2+}$  dynamics on the genesis of subcellular  $\text{Ca}^{2+}$  alternans: L-type  $\text{Ca}^{2+}$  channels and  $\text{Ca}^{2+}$  buffers.

The L-type  $\text{Ca}^{2+}$  channel has received significant attention due to its central role in excitation-contraction coupling [27–30]. Its contribution to the formation of  $\text{Ca}^{2+}$  alternans is ambiguous though [31]. On the one hand, several studies have provided compelling evidence that altering the dynamics of L-type  $\text{Ca}^{2+}$  channel through e.g. cooperative gating or reducing the current can either promote or inhibit  $\text{Ca}^{2+}$  alternans [32,33]. On the other hand,  $\text{Ca}^{2+}$  alternans have been observed with clamped membrane voltage, thus limiting the degree of control that L-type  $\text{Ca}^{2+}$  channels can exert on the genesis of  $\text{Ca}^{2+}$  alternans [34]. Here, we investigate the role of  $\text{Ca}^{2+}$ -dependent inactivation of the L-type  $\text{Ca}^{2+}$  channel on the dynamics of a CRU, which occurs in addition to voltage-dependent activation and inactivation [35,36]. We find that  $\text{Ca}^{2+}$ -dependent inactivation affects the formation of subcellular  $\text{Ca}^{2+}$  alternans in a nontrivial manner that depends on the unitary current of the L-type  $\text{Ca}^{2+}$  channel.

$\text{Ca}^{2+}$  buffers are essential for cardiac function, not least because activation of the cytoplasmic buffer troponin C determines how strongly a cardiac myocyte contracts [27,37]. In addition, the buffers calsequestrin and calmodulin have been shown to vitally shape the dynamics of cardiac myocyte including an impact on the refractoriness of RyRs [38–52]. As has been demonstrated both experimentally and theoretically for numerous cell types and  $\text{Ca}^{2+}$  releasing channels, including the inositol-1,4,5-trisphosphate receptor,  $\text{Ca}^{2+}$  buffers can fundamentally alter the dynamics of intracellular  $\text{Ca}^{2+}$  dynamics ranging from local  $\text{Ca}^{2+}$  release events such as  $\text{Ca}^{2+}$  sparks and  $\text{Ca}^{2+}$  puffs to global  $\text{Ca}^{2+}$  patterns such as travelling  $\text{Ca}^{2+}$  waves. Due to the nonlinear dynamics of  $\text{Ca}^{2+}$  buffers, direct predictions are difficult to make. We show through numerical simulations that  $\text{Ca}^{2+}$  buffers can both promote and inhibit subcellular  $\text{Ca}^{2+}$  alternans, which adds another facet to the already rich repertoire of buffered  $\text{Ca}^{2+}$  dynamics.

## 2. Materials and methods

We consider a two-dimensional network of  $15 \times 10$  CRUs corresponding to a transversal cut along a z-plane. We assume that CRUs are structurally identical, but note recent experimental evidence of heterogeneity amongst CRUs [53]. The dynamics of a CRU with label  $\mu$  is governed by the Shiferaw-Karma model [34]

$$\frac{dc_s^\mu}{dt} = \beta(c_s^\mu) \left[ \frac{v_i}{v_s} \left( I_r^\mu - \frac{c_s^\mu - c_i^\mu}{\tau_s} - I_{\text{CaL}}^\mu \right) + I_{\text{NCX}}^\mu \right], \quad (1a)$$

$$\frac{dc_i^\mu}{dt} = \beta(c_i^\mu) \left[ \frac{c_s^\mu - c_i^\mu}{\tau_s} - I_{\text{up}}^\mu \right] + \sum_{\eta \in \mathcal{I}_n} \frac{c_i^\eta - c_i^\mu}{\tau_c}, \quad (1b)$$

$$\frac{dc_j^\mu}{dt} = -I_r^\mu + I_{up}^\mu + \sum_{\eta \in \mathcal{I}_n} \frac{c_j^\eta - c_j^\mu}{\tau_{sr}}, \quad (1c)$$

$$\frac{dc_u^\mu}{dt} = \frac{c_j^\mu - c_u^\mu}{\tau_a}, \quad (1d)$$

$$\frac{dI_r^\mu}{dt} = -gI_{CaL}Q(c_u^\mu) - \frac{I_r^\mu}{\tau_r}. \quad (1e)$$

The  $\text{Ca}^{2+}$  concentrations in the subsarcolemmal space and in the cytosolic bulk are denoted by  $c_s^\mu$  and  $c_i^\mu$ , respectively, while the total  $\text{Ca}^{2+}$  concentration in the SR and the  $\text{Ca}^{2+}$  concentration in the unrecruited SR are given by  $c_j^\mu$  and  $c_u^\mu$ , respectively. The  $\text{Ca}^{2+}$  release current from the unrecruited SR into the subsarcolemmal space is  $I_r^\mu$ , and we refer to the L-type  $\text{Ca}^{2+}$  current, the NCX current and the SERCA uptake current by  $I_{CaL}^\mu$ ,  $I_{NCX}^\mu$  and  $I_{up}^\mu$ , respectively. The model contains four diffusive currents with timescales  $\tau_s$ ,  $\tau_c$ ,  $\tau_{sr}$  and  $\tau_a$ , describing coupling between the subsarcolemmal space and the cytosolic bulk, through the cytosolic bulk between neighbouring CRUs (indexed by  $\mathcal{I}_n$ ), between the total and unrecruited SR, and through the SR between neighbouring CRUs (indexed by  $\mathcal{I}_n$ ), respectively. Note that each CRU is coupled to its four nearest neighbours. In some instances, we report the network coupling strengths as inverse of the timescales, i.e.  $\sigma_x = \tau_x^{-1}$ ,  $x \in \{c, sr\}$ . The L-type  $\text{Ca}^{2+}$  current is modelled as  $I_{CaL}^\mu = I_{Ca}^\mu P_o$  with

$$I_{Ca}^\mu = 4i_{Ca}P_{Ca}F\alpha \frac{c_s^\mu \times 10^{-3} \exp(2\alpha) - \gamma_0 Ca_o}{\exp(2\alpha) - 1}, \quad (2)$$

where  $\alpha = FV/RT$ ,  $i_{Ca}$  is the parameter that we vary to control the strength of the L-type  $\text{Ca}^{2+}$  current and  $P_o = dqf$  is the open probability. Here,  $d$  is the value of the fast voltage-dependent activation gate,  $q$  corresponds to the  $\text{Ca}^{2+}$ -dependent inactivation gate and  $f$  to the voltage-dependent inactivation gate. All gates are described by first order kinetics of the form

$$\frac{dx}{dt} = \frac{x_\infty - x}{\tau_x}, \quad x \in \{d, f, q\}. \quad (3)$$

Of particular interest for the present study is

$$q_\infty = \frac{c_e^\gamma}{c_e^\gamma + c_s^\gamma}, \quad (4)$$

where  $c_e$  sets the  $EC_{50}$  value, i.e. the value of the subsarcolemmal  $\text{Ca}^{2+}$  concentration  $c_s$  at which  $q_\infty$  equals 0.5, and  $\gamma$  controls the sensitivity of  $\text{Ca}^{2+}$ -dependent inactivation. Essentially, the larger  $\gamma$  the more step-like the inactivation around a  $\text{Ca}^{2+}$  concentration of  $c_e$ . Following [34], we clamp the voltage for a pacing period  $T_p$  as

$$V(t) = \begin{cases} V_+(t), & kT_p \leq t \leq (k+x)T_p, \\ V_{\min}, & (k+x)T_p \leq t < (k+1)T_p, \end{cases} \quad (5)$$

where  $k \in \mathbb{N}$  counts the number of APs in the simulation and  $x = a_x/(a_x + T_p)$  with  $a_x = 2/3$ . The resting potential is given by  $V_{\min} = -70\text{mV}$ , and  $V_+(t)$  captures the shape of the clamped voltage, which is given by

$$V_+(t) = V_{\min} + (V_{\max} - V_{\min}) \sqrt{1 - \left( \frac{t - kT_p}{xT_p} \right)^2}. \quad (6)$$

Note that Eq. (6) is valid for  $kT_p \leq t \leq (k+x)T_p$  and that each CRU experiences the same voltage. The maximal AP is set at  $V_{\max} = 30\text{mV}$ . Buffering is modelled based on the fast-buffer approximation [54,55] yielding

$$\frac{1}{\beta(c)} = 1 + \frac{B_{SR}K_{SR}}{(c + K_{SR})^2} + \frac{B_TK_T}{(c + K_T)^2} + \frac{B_{Cd}K_{Cd}}{(c + K_{Cd})^2}, \quad (7)$$

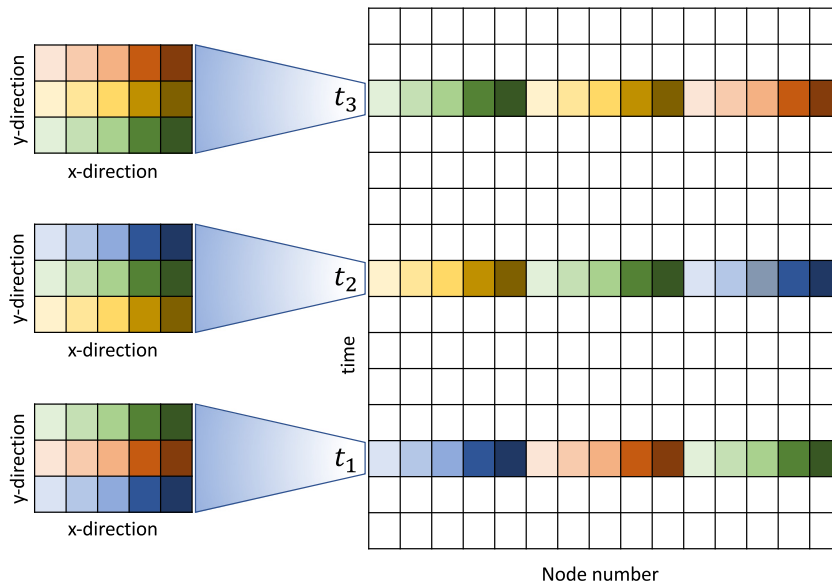
where  $B_{SR}$  denotes the total buffer concentration in the SR and  $K_{SR}$  the associated dissociation constant. Constants with the subscript T and Cd have the same interpretation, but correspond to troponin C and calmodulin, respectively. For all other details of the model including the functional forms  $i_{Ca}$  and  $I_{NCX}$ , we refer the reader to [34]. A list of all parameter values used in this study is provided in Table 1. We employ no-flux boundary conditions in all simulations.

### 3. Results

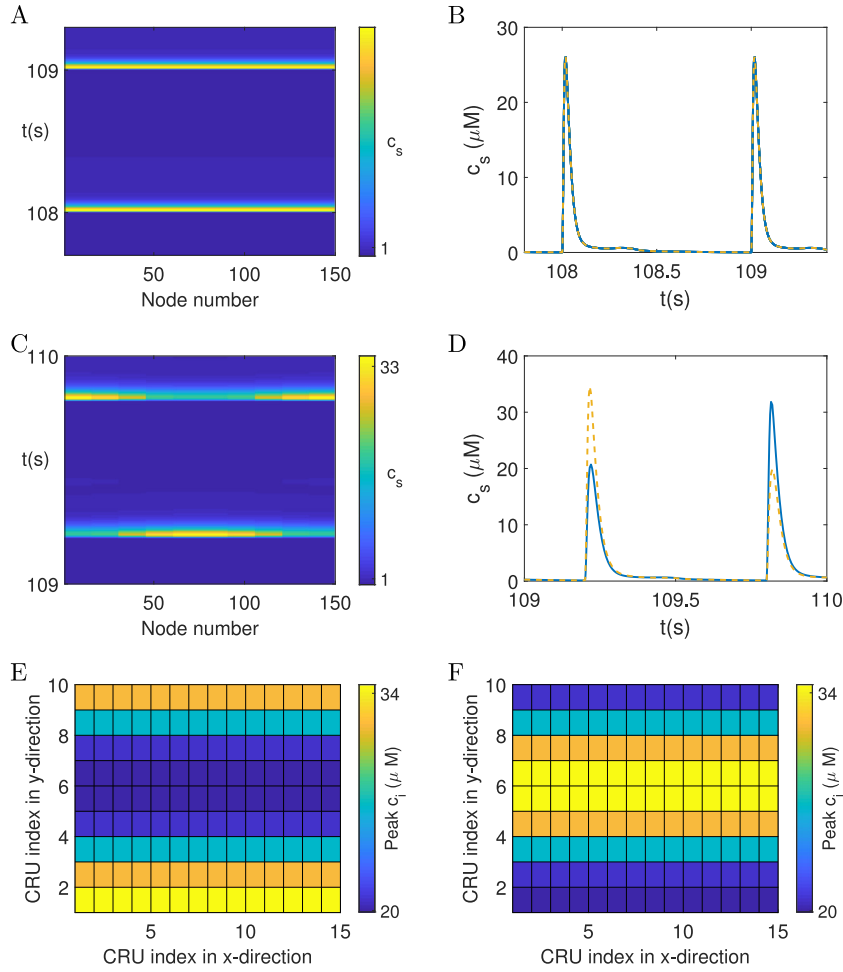
As this study focuses on subcellular  $\text{Ca}^{2+}$  alternans in two-dimensional CRU networks, we wish to visualise the  $\text{Ca}^{2+}$  concentration simultaneously across the two spatial dimensions and time. One way to achieve this is illustrated in Fig. 1 for a  $5 \times 3$  CRU network. On the left, we plot one component of the CRU model, e.g. the subsarcolemmal  $\text{Ca}^{2+}$  concentration or

**Table 1**  
Standard parameter values used in the study.

	Definition	Value
T	Temperature	308 K
F	Faraday's constant	96.4867 C/mmol
R	Gas constant	8.314 J/K mol
Na <sub>o</sub>	External sodium concentration	140 mM
Ca <sub>o</sub>	External calcium concentration	1.8 mM
$v_s/v_i$	Subsarcolemmal/cell volume	0.1
$c_{up}$	Uptake threshold	0.5 $\mu$ M
$v_{up}$	Uptake strength	270 $\mu$ M/s
$\tilde{I}_{NaCa}$	Strength of the NaCa exchanger	10 <sup>5</sup> $\mu$ M/s
$k_{sat}$	Constant from the 1994 Luo-Rudy model	0.1
$\xi$	Constant from the 1994 Luo-Rudy model	0.35
$K_{mNa}$	Constant from the 1994 Luo-Rudy model	87.5 mM
$K_{mCa}$	Constant from the 1994 Luo-Rudy model	1.38 mM
$\gamma_s$	Constant from the 1994 Luo-Rudy model	1
$\gamma_o$	Constant from the 1994 Luo-Rudy model	0.341
$P_{Ca}$	Constant from the 1994 Luo-Rudy model	$5.4 \times 10^{-4}$ cm/s
$i_{Ca}$	Flux constant	6600 $\mu$ mol/C cm
$\tau_f$	Time constant for voltage-dependent inactivation	30 ms
$\tau_d$	Time constant for voltage-dependent activation	5 ms
$\tau_q$	Time constant for Ca <sup>2+</sup> -dependent inactivation	20 ms
$\tilde{c}_c$	Calcium inactivation threshold	0.5 $\mu$ M
$\gamma$	Sensitivity parameter for calcium dependent inactivation	4
$g$	Release current strength	$3.5 \times 10^4$ sparks/ $\mu$ M
$u$	Release slope	11.3 s <sup>-1</sup>
$\tau_r$	Average spark life time	20 ms
$\tau_a$	Relaxation time of $c_u$ to $c_j$	50 ms
$\tau_s$	Submembrane diffusion time constant	10 ms
$B_T$	Total concentration of troponin C binding sites	70 $\mu$ mol/1 cytosol
$B_{SR}$	Total concentration of SR binding sites	47 $\mu$ mol/1 cytosol
$B_{Cd}$	Total concentration of calmodulin binding sites	24 $\mu$ mol/1 cytosol
$K_T$	Dissociation constant for troponin C binding sites	0.6 $\mu$ M
$K_{SR}$	Dissociation constant for SR binding sites	0.6 $\mu$ M
$K_{Cd}$	Dissociation constant for calmodulin binding sites	7 $\mu$ M
$\beta_s$	Buffering constant for $c_s$	0.5
$\beta_i$	Buffering constant for $c_i$	0.01
$\sigma_c$	Coupling strength in cytosol	1 s <sup>-1</sup>
$\sigma_c$	Coupling strength in the SR	30 s <sup>-1</sup>



**Fig. 1.** Schematic showing the spatio-temporal visualisation of Ca<sup>2+</sup> concentrations across a 5 × 3 CRU network. The three networks on the left represent the Ca<sup>2+</sup> concentration for one node component of the CRU network at three different times  $t_1 < t_2 < t_3$ . The right plot corresponds to a space-time plot where space runs horizontally (represented as node number) and time vertically. See text for details.

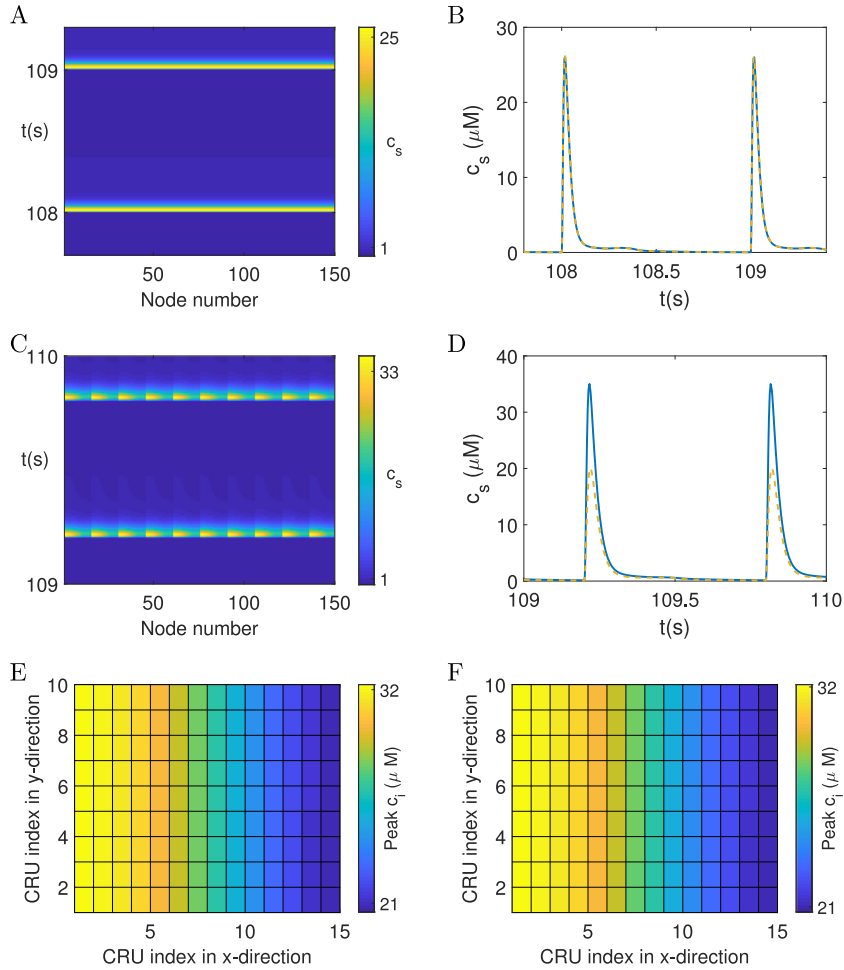


**Fig. 2.** Space-time plots of the unravelled CRU network (A,C) and time traces (B,D) of the subsarcolemmal  $\text{Ca}^{2+}$  concentration for  $T_p = 1$  s (A,B) and  $T_p = 0.6$  s (C,D). The colouring in (B,D) refers to node 25 (solid blue) and 75 (dashed yellow). (E,F) Peak subsarcolemmal  $\text{Ca}^{2+}$  concentration on two successive beats across the CRU network for the data shown in (C). Parameter values as in Table 1 and  $\sigma_c = 15 \text{ s}^{-1}$ ,  $\sigma_{sr} = 3 \text{ s}^{-1}$ . (For interpretation of the references to colour in this figure legend, the reader is referred to the web version of this article.)

the  $\text{Ca}^{2+}$  concentration in the cytosolic bulk, at different times  $t_1 < t_2 < t_3$ . Each coloured box corresponds to one CRU, and the colour encodes the value of the CRU component. Note that the colour scheme is chosen for illustrative purposes only.

Each snapshot of the two-dimensional CRU network can be transformed into a one-dimensional representation by sequentially taking rows of the two-dimensional network from bottom to top and concatenating them horizontally from left to right. For instance, consider the network state at time  $t_1$  shown on the left. We first take the row at the bottom (blue colours), which we amend from the right with the second row (orange colours) followed by the top row (green colours) to obtain the one-dimensional representation shown on the right. The order of elements within each row of the two-dimensional CRU network is conserved, as indicated by the same order of colours within each block of the same base colour, i.e. blue, orange and green. These one-dimensional representation are then stacked vertically to produce a space-time plot as shown on the right of Fig. 1. Here, space runs horizontally, represented as node number, and time runs from bottom to top. The node number is assigned by enumerating CRUs sequentially starting with the bottom left CRU in the two-dimensional network. We then proceed along the row towards the right increasing the node number by one until we reach the end of that row. We then continue with the left-most CRU in the next row above, again moving left to right.

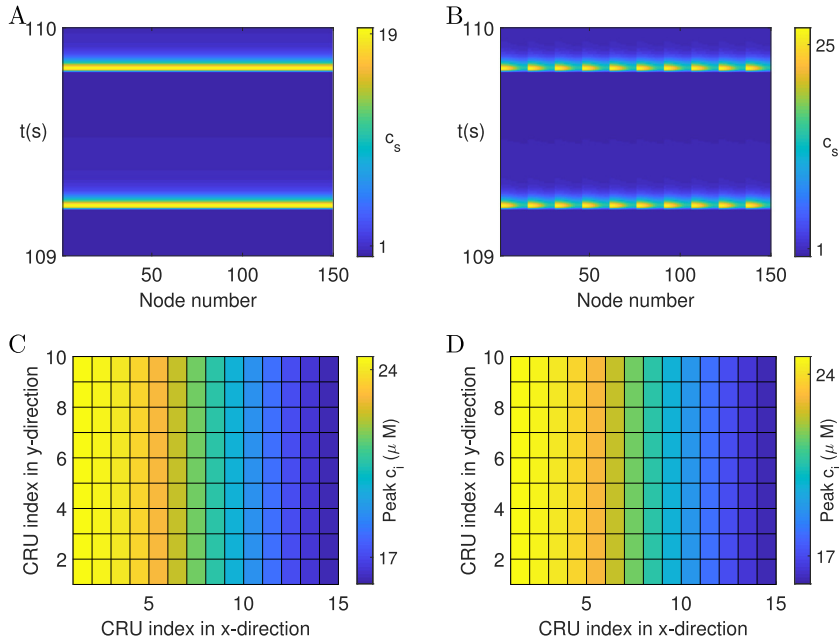
To establish a baseline for our findings, we first investigate the dynamics of the CRU network when buffers are clamped over time. In other words, we set  $\beta(c_s^\mu) \equiv \beta_s = \text{const}$  and  $\beta(c_i^\mu) \equiv \beta_i = \text{const}$  for all  $\mu$ . When cytosolic coupling is dominant, i.e.  $\tau_c \ll \tau_{sr}$  ( $\sigma_c \gg \sigma_{sr}$ ), synchrony is stable for low pacing frequencies as demonstrated in Fig. 2A. We here show a space-time plot of the *unravelled* CRU network as introduced above. The existence of stable synchronous network solutions can be inferred from these representations by the absence of any horizontal variation in colouring: each CRU exhibits identical behaviour. Fig. 2B makes this explicit by showing the temporal evolution of the subsarcolemmal  $\text{Ca}^{2+}$  concentration at nodes 25 and 75. The two curves lie on top of each other. The results in Fig. 2 as well as all other data presented in this study



**Fig. 3.** Space-time plots of the unravelled CRU network (A,C) and time traces (B,D) of the subsarcolemmal  $\text{Ca}^{2+}$  concentration for  $T_p = 1$  s (A,B) and  $T_p = 0.6$  s (C,D). The colouring in (B,D) refers to node 31 (solid blue) and 75 (dashed yellow). (E,F) Peak subsarcolemmal  $\text{Ca}^{2+}$  concentration on two successive beats across the CRU network for the data shown in (C). Parameter values as in Table 1 and  $\sigma_c = 2 \text{ s}^{-1}$ ,  $\sigma_{sr} = 30 \text{ s}^{-1}$ . (For interpretation of the references to colour in this figure legend, the reader is referred to the web version of this article.)

are obtained after a sufficiently long simulation time so that initial transients have decayed and the system is at steady state. For instance, the data in Fig. 2A depicts the subsarcolemmal  $\text{Ca}^{2+}$  concentration for beats 181 and 182. When we decrease  $T_p$ , we observe the emergence of subcellular  $\text{Ca}^{2+}$  alternans as depicted in Fig. 2C. Each CRU follows a period-2 orbit, where a small amplitude  $\text{Ca}^{2+}$  transient on one beat is followed by a large  $\text{Ca}^{2+}$  transient on the next beat. Consider the node with number 75. During the first stimulus (around 109.2 s) we observe a large transient indicated by the yellow colour. On the next beat at around 109.8 s, the same node exhibits a much smaller transient as can be gleaned from the bluish colour. The behaviour is reversed for node 25, which first exhibits a small amplitude transient, followed by a large amplitude transient. This is shown explicitly in Fig. 2D, where we again plot the time traces of the subsarcolemmal  $\text{Ca}^{2+}$  concentration at these two nodes. Fig. 2E and F provide a more detailed view on the emergent spatial  $\text{Ca}^{2+}$  pattern. We plot the peak subsarcolemmal  $\text{Ca}^{2+}$  concentration on two successive beats. Since CRUs obtain their individual maximal values at the same time during one beat, Fig. 2E and F correspond to snapshots of the subsarcolemmal  $\text{Ca}^{2+}$  concentration across the entire CRU network at these maximal peak times. The  $\text{Ca}^{2+}$  alternans are arranged in an *inside-out* pattern along the long axis of the network, where CRUs within one row show almost identical behaviour, but peak amplitudes vary along the vertical direction. When  $\text{Ca}^{2+}$  transients are large in the centre, they are small towards the top and bottom. On the next beat, this pattern is reversed with large  $\text{Ca}^{2+}$  transients at the top and bottom.

For dominant luminal coupling, where  $\tau_c \gg \tau_{sr}$  ( $\sigma_c \ll \sigma_{sr}$ ), we again find stable synchrony at low pacing frequencies (see Fig. 3A and B). Indeed, the space-time plot and the time traces of the subsarcolemmal  $\text{Ca}^{2+}$  concentration are identical to the those in Fig. 2A and B, since when all CRUs exhibit the same behaviour, the coupling terms in Eqs. (1b) and (1c) vanish. The main difference between dominant cytosolic and dominant luminal coupling becomes apparent when we lower  $T_p$ . For the latter, we find subcellular  $\text{Ca}^{2+}$  alternans that emerge via a saddle-node bifurcation at the network level, in contrast to



**Fig. 4.** Space-time plot of the subarcolemmal  $\text{Ca}^{2+}$  concentration of the unravelled CRU network for  $i_{\text{Ca}} = 4400 \mu\text{mol C}^{-1}\text{cm}^{-1}$  and (A)  $\gamma = 1$ , (B)  $\gamma = 3$ . (C,D) Peak subarcolemmal  $\text{Ca}^{2+}$  concentration on two successive beats across the CRU network. Parameter values as in (B). For all other parameter values, see Table 1.

a period doubling bifurcation for the former. As Fig. 3C and D highlight, each CRU follows a period-1 orbit, but this orbit differs amongst the CRUs in the network. Fig. 3E and F show the peak subarcolemmal  $\text{Ca}^{2+}$  concentration during one beat across the CRU network and illustrate that CRUs on the left form large  $\text{Ca}^{2+}$  amplitude transients, while the transients are smaller towards the right. In the following we will use Fig. 3C–F as a reference case and contrast them with the network behaviour when we alter the behaviour of the L-type  $\text{Ca}^{2+}$  channel and that of  $\text{Ca}^{2+}$  buffers.

### 3.1. L-type $\text{Ca}^{2+}$ channel

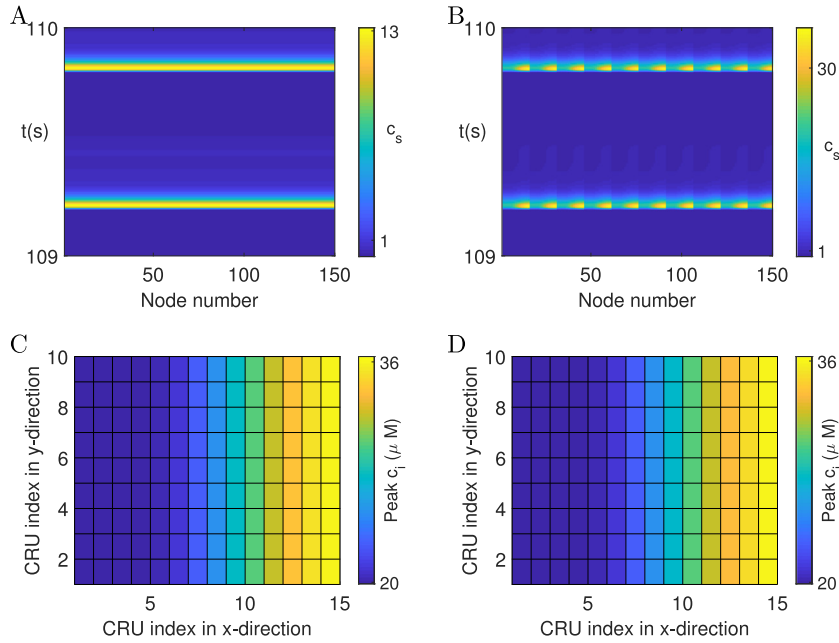
The extent to which  $\text{Ca}^{2+}$ -dependent inactivation sets in as a function of the subarcolemmal  $\text{Ca}^{2+}$  concentration  $c_s^\mu$  is controlled by the exponent  $\gamma$  in Eq. (4). When  $\gamma$  is small, the inverse Hill function  $q_\infty$  drops slowly from 1 to 0, while a large value of  $\gamma$  leads to switch-like behaviour around a concentration value of  $c_e$ . As Fig. 4A illustrates, the synchronous network state is stable when  $\gamma$  is small. On the other hand, as  $\gamma$  is increased, subcellular  $\text{Ca}^{2+}$  alternans emerge via a saddle-node bifurcation as shown in Fig. 4B–D. Fig. 4B displays a space-time plot of the unravelled CRU network where the variation of the maxima of the  $\text{Ca}^{2+}$  transients is clearly visible as the colour changes from yellow to blue when we traverse the network. We can also discern changes in the duration of the  $\text{Ca}^{2+}$  transient as evidenced by the wedge shape of the yellow regions of increased  $\text{Ca}^{2+}$ . Fig. 4C and D provide more detail on the spatial pattern of the subcellular  $\text{Ca}^{2+}$  alternans. On each beat, large  $\text{Ca}^{2+}$  transients occur towards the left side of the myocyte, while  $\text{Ca}^{2+}$  transients are small towards the right side. Note that there is no variation of the  $\text{Ca}^{2+}$  peak amplitudes along the y-direction. These results suggest that a more gradual  $\text{Ca}^{2+}$ -dependent inhibition of the L-type  $\text{Ca}^{2+}$  channel, i.e. when  $\gamma$  is small, protects cardiac myocytes from subcellular  $\text{Ca}^{2+}$  alternans.

The unitary current of an L-type  $\text{Ca}^{2+}$  channel can be modulated through various mechanisms, including  $\beta$ -adrenergic stimulation. The space-time plot in Fig. 5A shows that for small values of  $i_{\text{Ca}}$ , synchrony is stable. However, upon increasing the single channel current, subcellular  $\text{Ca}^{2+}$  alternans emerge via a saddle-node bifurcation as illustrated in Fig. 5B. The  $\text{Ca}^{2+}$  pattern is identical to the one found in Fig. 4 in that the  $\text{Ca}^{2+}$  concentration remains constant vertically but varies horizontally, see Fig. 5C and D. The fact that the large  $\text{Ca}^{2+}$  transients occur towards the right in Fig. 5C and D as apposed to the left in Fig. 4C and D is due to initial conditions. Overall, the results plotted in Fig. 5 are consistent with experimental findings that upregulation of the L-type  $\text{Ca}^{2+}$  channel is pro-arrhythmogenic [33].

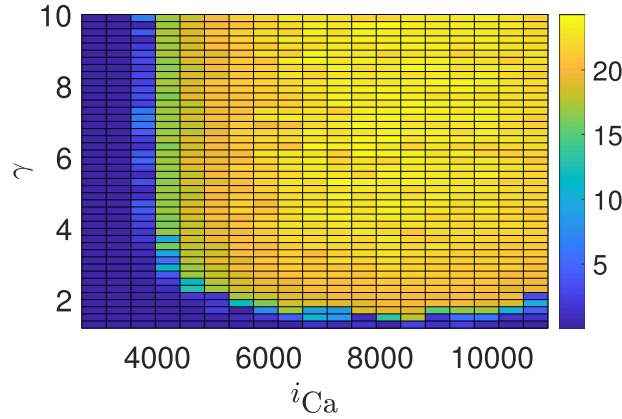
The  $\text{Ca}^{2+}$  profiles depicted in Figs. 4 and 5 suggest that the effect of the unitary L-type  $\text{Ca}^{2+}$  current on the generation of subcellular  $\text{Ca}^{2+}$  alternans depends on the properties of  $\text{Ca}^{2+}$ -dependent inactivation of the channel and vice versa. In Fig. 6 we provide a more comprehensive view on the interplay between these two components. For a given pair of  $\gamma$  and  $i_{\text{Ca}}$ , we compute the maximal difference in peak subarcolemmal  $\text{Ca}^{2+}$  on successive beats for a CRU with index  $\mu$ , i.e.

$$\theta^\mu = \max_i |c_s^{\mu,i} - c_s^{\mu,i+1}|, \quad (8)$$





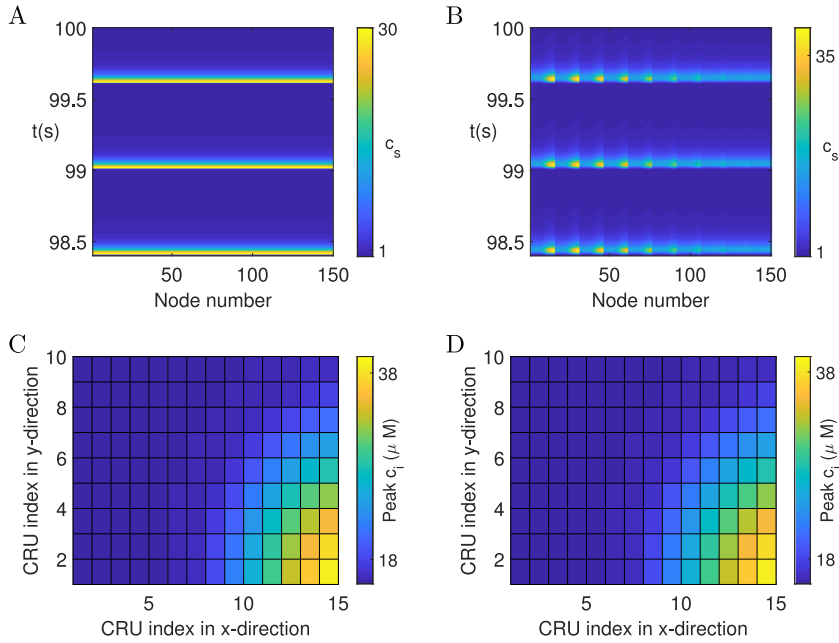
**Fig. 5.** Space-time plot of the subsarcolemmal  $\text{Ca}^{2+}$  concentration of the unravelled CRU network for  $\gamma = 3$  and (A)  $i_{\text{Ca}} = 2200 \mu\text{mol C}^{-1}\text{cm}^{-1}$ , (B)  $i_{\text{Ca}} = 6600 \mu\text{mol C}^{-1}\text{cm}^{-1}$ . (C,D) Peak subsarcolemmal  $\text{Ca}^{2+}$  concentration on two successive beats across the CRU network. Parameter values as in (B). For all other parameter values, see Table 1.



**Fig. 6.** Maximal beat-to-beat variation  $\theta$  of the subsarcolemmal  $\text{Ca}^{2+}$  concentration as a function of  $\gamma$  and  $i_{\text{Ca}}$ . All other parameter values as in Table 1.

where  $c_s^{\mu,i}$  is the maximum of  $c_s^{\mu}$  on the  $i$ th beat. Then, we determine the maximum of all  $\theta^{\mu}$  across the CRU network,  $\theta = \max_{\mu} \theta^{\mu}$ . When  $i_{\text{Ca}}$  is small,  $\theta$  vanishes irrespective of the value of  $\gamma$ , indicating that synchrony is stable and does not depend on how quickly  $\text{Ca}^{2+}$ -dependent inactivation sets in. For larger values of  $i_{\text{Ca}}$ , we observe a sharp transition from synchrony (blue) to alternans (yellow) upon increase of  $\gamma$ . Hence, for a sufficiently strong unitary L-type  $\text{Ca}^{2+}$  current, subcellular  $\text{Ca}^{2+}$  alternans can be induced if  $\text{Ca}^{2+}$ -dependent inactivation becomes more switch-like. When  $\text{Ca}^{2+}$ -dependent inactivation sets in more gradually, i.e.  $\gamma$  is small, synchrony is stable as we increase  $i_{\text{Ca}}$ . However, for larger values of  $\gamma$ , we observe a sharp transition from synchrony to subcellular  $\text{Ca}^{2+}$  alternans as the L-type  $\text{Ca}^{2+}$  channel becomes stronger. There appears to be an L-shape stability boundary in that for a large range of  $\gamma$ , subcellular  $\text{Ca}^{2+}$  alternans appear for approximately the same value of  $i_{\text{Ca}}$ , while for a large range of  $i_{\text{Ca}}$ , alternans set in for approximately the same small value of  $\gamma$ . We also note that the transition from stable synchrony to subcellular  $\text{Ca}^{2+}$  alternans is quite abrupt, as indicated by the sharp transition from blue to yellow. Taken together, our findings provide strong evidence that the L-type  $\text{Ca}^{2+}$  channel can initiate subcellular  $\text{Ca}^{2+}$  alternans, either via its  $\text{Ca}^{2+}$ -dependent inactivation or the strength of its unitary  $\text{Ca}^{2+}$  current.



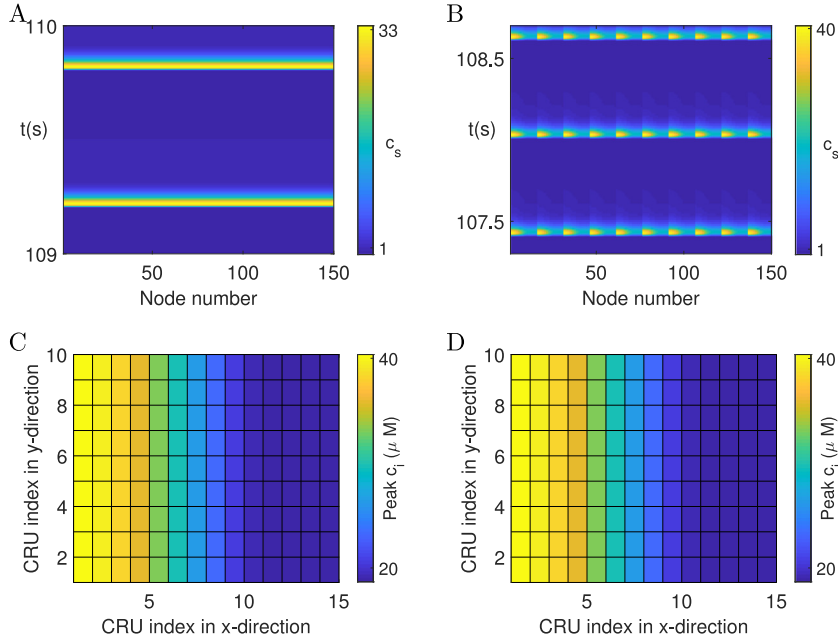


**Fig. 7.** Space-time plot of the subsarcolemmal  $\text{Ca}^{2+}$  concentration of the unravelled CRU network for (A) fully nonlinear buffers and (B) desensitised buffers. (C,D) Peak subsarcolemmal  $\text{Ca}^{2+}$  concentration on two successive beats across the CRU network. Parameter values as in (B). Other parameter values as in Table 1 and  $K_{SR} = 6.0 \mu\text{M}$ ,  $K_T = 600.0 \mu\text{M}$ ,  $K_{Cd} = 7.0 \mu\text{M}$ ,  $B_{SR} = 250.0 \mu\text{mol/l}$  cytosol,  $B_T = 12000.0 \mu\text{mol/l}$  cytosol,  $B_{Cd} = 1.0 \mu\text{mol/l}$  cytosol.

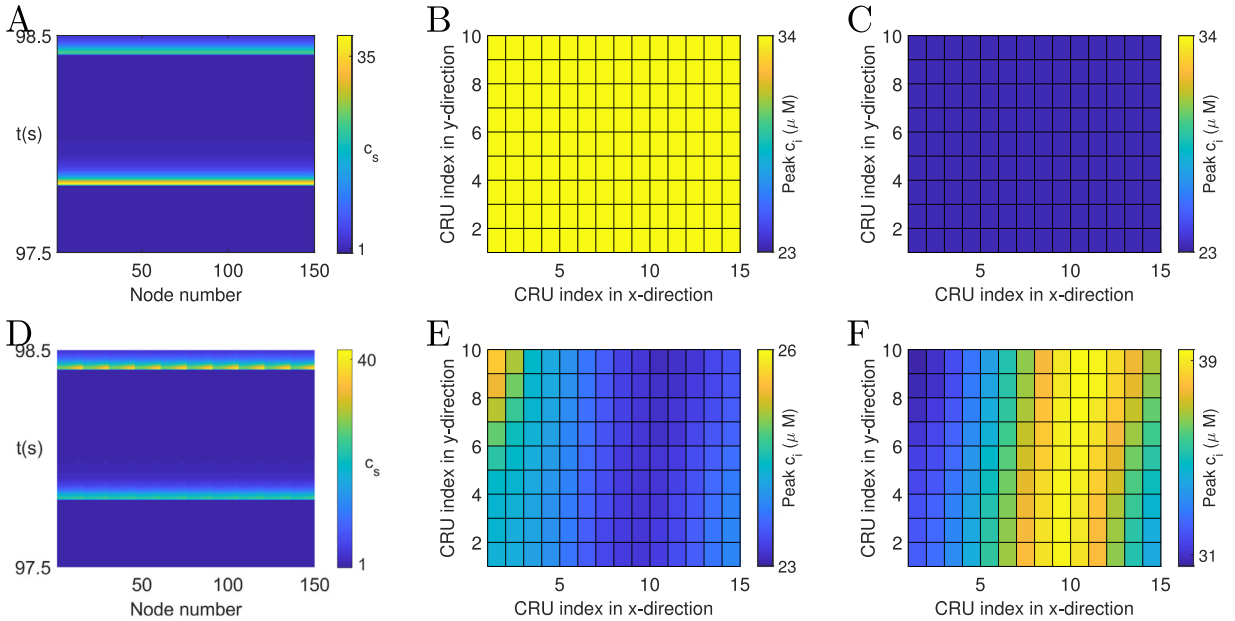
#### 4. Buffers

All results so far were obtained for constant buffer contributions. In other words, we set  $\beta(c_i^\mu)$  and  $\beta(c_s^\mu)$  to constants  $\beta_i$  and  $\beta_s$ , respectively, consistent with earlier work [14]. In this way, we eliminate any time-dependent modulation of the  $\text{Ca}^{2+}$  dynamics through binding and unbinding to  $\text{Ca}^{2+}$  buffers. Under more general conditions, however, Eq. (7) entails that  $\beta(c_i^\mu)$  and  $\beta(c_s^\mu)$  oscillate with the same frequency as  $c_i^\mu$  and  $c_s^\mu$ , respectively. Fig. 7A illustrates that in this case, subcellular  $\text{Ca}^{2+}$  alternans can be abolished and synchrony is stable. This behaviour needs to be contrasted with that depicted in Fig. 5B, which we would obtain with the parameter values used in Fig. 7A upon replacing the dynamic buffers with the constant buffers used in Fig. 5B. In other words, while the dynamics of the L-type  $\text{Ca}^{2+}$  channel can induce subcellular  $\text{Ca}^{2+}$  alternans (as demonstrated in Fig. 5), dynamic  $\text{Ca}^{2+}$  buffers can rescue this pathological behaviour. This discrepancy between constant and time-dependent buffers prompted us to explore another form of non-responsive buffers. The sensitivity of buffers is usually determined by their dissociation constants, which in the present study are the three constants  $K_{SR}$ ,  $K_{Cd}$  and  $K_T$  in Eq. (7), as well as the corresponding concentration of binding sites  $B_{SR}$ ,  $B_{Cd}$  and  $B_T$ . By choosing appropriate values, we can effectively “desensitise” the  $\text{Ca}^{2+}$  buffers. As Fig. 7B–D illustrate for the desensitised dynamics, subcellular  $\text{Ca}^{2+}$  alternans re-emerge consistent with a saddle-node bifurcation. Fig. 7B shows a space-time plot of the unravelled CRU network. Each CRU follows a period-1 orbit, which differs both in amplitude and duration of the  $\text{Ca}^{2+}$  transient across the network, as can be deduced from the variation of the yellow wedges. A more detailed view on the spatial pattern is provided in Fig. 7C and D, which depict peak amplitudes of the subsarcolemmal  $\text{Ca}^{2+}$  concentration on successive beats. Note that although the subcellular  $\text{Ca}^{2+}$  alternans emerge through a saddle-node bifurcation, the spatial pattern differs from that observed in Figs. 4 and 5. This is consistent with our earlier findings, which have demonstrated a rich pattern space of subcellular  $\text{Ca}^{2+}$  alternans [15,16].

At this point, one might be tempted to conclude that constant buffers make the occurrence of subcellular  $\text{Ca}^{2+}$  alternans more likely. However, as Fig. 8A reveals, this is not the case. Leaving all parameter values unchanged but setting  $\beta_s = \beta_i = 1$  we find synchrony. Crucially, these simulations correspond to the case without buffers and should be contrasted with the results in Fig. 7A. In both cases, synchrony is stable, but the reasons as to why might differ. The constant values for  $\beta_s$  and  $\beta_i$  that we used in Section 3.1 were obtained for a piecewise linear (PWL) caricature of the model given by Eq. (1), see [14] for details. To obtain estimates that are more consistent with the full nonlinear model, we determine the mean values of  $\beta(c_s^\mu)$  and  $\beta(c_i^\mu)$  when synchrony is stable and assign them to  $\beta_s$  and  $\beta_i$ , respectively. For these values, we find subcellular  $\text{Ca}^{2+}$  alternans that are consistent with a saddle-node bifurcation as shown in Fig. 8B. Again, individual CRUs display a period-1 orbit, which differs throughout the network. The spatial pattern of the subcellular  $\text{Ca}^{2+}$  alternans is reminiscent of the one depicted in Fig. 4B–D, where  $\text{Ca}^{2+}$  transients are more pronounced on the left side of the CRU network compared to the right side.

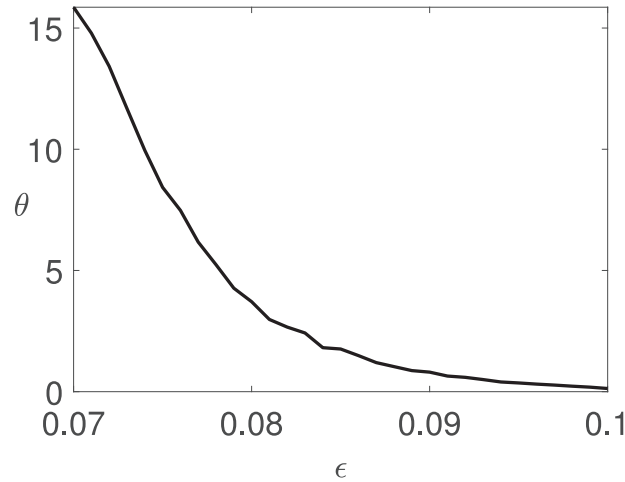


**Fig. 8.** Space-time plot of the subarcolemmal  $\text{Ca}^{2+}$  concentration of the unravelled CRU network for  $T_p = 0.6$  s and (A)  $\beta_s = \beta_i = 1$ , (B)  $\beta_s = 0.08827$ ,  $\beta_i = 0.01738$ . (C,D) Peak subarcolemmal  $\text{Ca}^{2+}$  concentration on two successive beats across the CRU network. Parameter values as in (B). For all other parameter values, see Table 1.



**Fig. 9.** Network dynamics for  $T_p = 0.6$  s and clamped nonlinear buffers for (A–C)  $\sigma_{sr} = 30$  s $^{-1}$ ,  $\sigma_c = 1$  s $^{-1}$ , (D–F)  $\sigma_{sr} = 3$  s $^{-1}$ ,  $\sigma_c = 0$  s $^{-1}$ . Space-time plots of the subarcolemmal  $\text{Ca}^{2+}$  concentration of the unravelled CRU are shown in (A) and (D). Peak subarcolemmal  $\text{Ca}^{2+}$  concentration on two successive beats across the CRU network are plotted in (B,C) and (E,F). For all other parameter values, see Table 1.

Since constant  $\text{Ca}^{2+}$  buffers can both promote as well as abolish subcellular  $\text{Ca}^{2+}$  alternans, we next explore the impact of the buffer time course on the formation of subcellular  $\text{Ca}^{2+}$  alternans. To do this in a controlled fashion, we extract the time course of both  $\beta(c_s^\mu)$  and  $\beta(c_i^\mu)$  from the full nonlinear model and then clamp the buffer time courses at each node to these profiles. In other words, each node experiences nonlinear buffer dynamics, but the buffers do not alternate from node to node. As Fig. 9A reveals, we obtain subcellular  $\text{Ca}^{2+}$  alternans that differ from those reported so far in this study. Here, every node in the network follows the same period-2 orbit characteristic of subcellular  $\text{Ca}^{2+}$  alternans that



**Fig. 10.** Maximal beat-to-beat variation  $\theta$  of the subsarcolemmal  $\text{Ca}^{2+}$  concentration as a function of the variability of the  $\text{Ca}^{2+}$  buffer  $\varepsilon$ . See text for details. Parameter values as in Table 1.

emerge via a period-doubling bifurcation. Fig. 9B and C illustrate the uniform behaviour across the network that alternates between successive beats. This spatial pattern is known as spatially concordant  $\text{Ca}^{2+}$  alternans. When we change the coupling strengths, but keep all other parameter values unaltered, we observe spatially discordant  $\text{Ca}^{2+}$  alternans as plotted in Fig. 9D–F. Every node follows a period-2 orbit, but different parts of the network oscillate out-of-phase with each other.

Our results so far strongly suggest that the time course and amplitude of  $\text{Ca}^{2+}$  buffers significantly impacts on the genesis of subcellular  $\text{Ca}^{2+}$  alternans. Fig. 10 shows results from an *in silico* experiment in which we tune the  $\text{Ca}^{2+}$  buffer dynamics from constant ( $\varepsilon = 0$ ) to fully nonlinear ( $\varepsilon = 1$ ) by replacing the buffer factor  $\beta$  in Eqs. (1a) and (1b) with

$$\beta_x^\varepsilon = \varepsilon \beta(c_x) + (1 - \varepsilon) \beta_x, \quad x \in \{x, i\}, \quad (9)$$

with  $\beta(c_x)$  as in Eq. (7) and  $\beta_x$  as in Table 1. As a measure for the strength of subcellular  $\text{Ca}^{2+}$  alternans, we report the maximal beat-to-beat variation  $\theta$  as defined after Eq. (8). As  $\varepsilon$  increases, we find a monotonic decrease in  $\theta$ , highlighting that nonlinear buffers have the potential to abolish subcellular  $\text{Ca}^{2+}$  alternans.

## 5. Discussion

Subcellular  $\text{Ca}^{2+}$  alternans have been firmly linked to the genesis of cardiac arrhythmias. Despite this crucial connection, we still lack a complete picture of how the dynamics of the intracellular  $\text{Ca}^{2+}$  concentration transitions from its healthy period-1 orbit to its various pathological forms.

Our focus has been on understanding subcellular  $\text{Ca}^{2+}$  alternans in tubulated myocytes, such as ventricular myocytes. The presence of t-tubules in these cells gives rise to well-defined CRUs, which form a network where nearest neighbours are coupled via  $\text{Ca}^{2+}$  diffusion, both through the cytosol and the SR. The discussion of whether  $\text{Ca}^{2+}$  diffusion in the SR is fast or slow has been ongoing for more than a decade [24–26], without a resolution in sight. We illustrate in Figs. 2 and 3 that whether  $\text{Ca}^{2+}$  diffuses more dominantly in the lumen or in the cytosol has major consequences for the spatial patterns of subcellular  $\text{Ca}^{2+}$  alternans. In the latter, subcellular  $\text{Ca}^{2+}$  alternans emerge via the classical period-doubling bifurcation, where CRUs exhibit a period-2 orbit and CRUs in different parts of the cell oscillate out-of-phase with each other. This behaviour has been well studied and documented [5–12]. On the other hand, when  $\text{Ca}^{2+}$  diffusion in the SR dominates, we observe a completely different spatial pattern originating from a saddle-node bifurcation. Here, CRUs show a period-1 orbit, which is different from the synchronous network state and where CRUs in different regions of the cell exhibit  $\text{Ca}^{2+}$  transients of varying amplitude. It is worth noting that the discussion of whether intraluminal  $\text{Ca}^{2+}$  diffusion is faster than cytosolic  $\text{Ca}^{2+}$  diffusion — a process known as intraluminal tunnelling — has already received attention, although in a different context [56]. Given the largely unexplored nature of the saddle-node bifurcation in the generation of subcellular  $\text{Ca}^{2+}$  alternans, we have concentrated on dominant luminal coupling in the present study and have investigated two main contributors that shape the dynamics of cardiac  $\text{Ca}^{2+}$ : the L-type  $\text{Ca}^{2+}$  channel and  $\text{Ca}^{2+}$  buffers.

The L-type  $\text{Ca}^{2+}$  channel constitutes a major  $\text{Ca}^{2+}$  conduit that regulates  $\text{Ca}^{2+}$  influx from the extracellular space into the myoplasm and is thus crucial for high-fidelity excitation-contraction coupling. It is therefore not surprising that pathologies of the L-type  $\text{Ca}^{2+}$  channel can lead to abnormal  $\text{Ca}^{2+}$  dynamics. When we increase the single channel  $\text{Ca}^{2+}$  current  $i_{\text{Ca}}$ , subcellular  $\text{Ca}^{2+}$  alternans are more likely to occur as evidenced by the transition from blue to yellow in Fig. 6. However, this behaviour depends on the strength of  $\text{Ca}^{2+}$ -dependent inactivation of the L-type  $\text{Ca}^{2+}$  channel. As is often the case, the inactivation gate is modelled via a first-order kinetic scheme with a time constant  $\tau_q$  and a state-dependent steady state  $q_\infty$ . As Eq. (4) shows,  $q_\infty$  follows an inverse Hill function with exponent  $\gamma$ . Hence, for small values of  $\gamma$ ,  $q_\infty$  changes gradually

as a function of the subsarcolemmal  $\text{Ca}^{2+}$  concentration  $c_s$ . On the other hand, large values of  $\gamma$  lead to a switch-like Hill function. When  $i_{\text{Ca}}$  is small, the increase in subsarcolemmal  $\text{Ca}^{2+}$  is small as well, which in turn almost completely eliminates  $\text{Ca}^{2+}$  dependent inactivation (as  $q$  never falls sufficiently towards zero). Therefore, we do not observe any effect of  $\gamma$  on the generation of subcellular  $\text{Ca}^{2+}$  alternans in this regime, indicated by the blue band towards the left of Fig. 6. On the other hand, as we increase  $i_{\text{Ca}}$ , the larger subsarcolemmal  $\text{Ca}^{2+}$  concentrations allow for a larger exploration of the right tail of  $q_\infty$ , and hence values closer to zero. When  $\gamma$  is large making  $q_\infty$  more step-like, bigger values of  $c_s^\mu$  entail longer periods where  $q$  tends to zero. An increase of  $i_{\text{Ca}}$  does not change that, meaning that the nature of the subcellular  $\text{Ca}^{2+}$  alternans is not affected by increasing  $i_{\text{Ca}}$  for larger values of  $\gamma$ . This explains the almost uniform yellow colouring in Fig. 6 for fixed large  $\gamma$  and varying  $i_{\text{Ca}}$ . An interesting feature of Fig. 6 is the sharp transition from regular behaviour to subcellular  $\text{Ca}^{2+}$  alternans as is manifest from the abrupt colour change from blue to yellow. It remains to be seen whether this behaviour can be understood more formally in terms of a phase transition.

All results for the L-type  $\text{Ca}^{2+}$  channel were obtained with constant buffer contributions. However, since the concentration of  $\text{Ca}^{2+}$  bound buffers directly depends on the intracellular  $\text{Ca}^{2+}$  concentration, the buffer function  $\beta$  in Eq. (7) should evolve over time. Using the full nonlinear buffers, we find that subcellular  $\text{Ca}^{2+}$  alternans are extinguished (Fig. 7A). In other words, solely changing the buffer dynamics completely alters the dynamics of the cardiac cell. These findings are in line with a large body of literature demonstrating that  $\text{Ca}^{2+}$  buffers can substantially modify intracellular  $\text{Ca}^{2+}$  dynamics. From a physiological perspective, our results indicate that  $\text{Ca}^{2+}$  buffers can perform a stabilising role that can compensate for dysfunctions of other components of the  $\text{Ca}^{2+}$  signalling toolkit, such as the L-type  $\text{Ca}^{2+}$  channel. Because  $\text{Ca}^{2+}$  buffers are slaved to the  $\text{Ca}^{2+}$  dynamics, the buffer dynamics exhibit alternans as soon as the intracellular  $\text{Ca}^{2+}$  concentration alternates. For the results in Fig. 9, we broke this connection and clamped the  $\text{Ca}^{2+}$  buffer dynamics in such a way that each node exhibits the same nonlinear orbit. In other words,  $\text{Ca}^{2+}$  buffers alternate at each node, but there is no spatial variation of the buffer dynamics. In this regime, the patterns of the subcellular  $\text{Ca}^{2+}$  alternans vary drastically from the ones we observed so far. We found spatially concordant alternans, which can transition into spatially discordant alternans upon altering the coupling strength of cytosolic and SR diffusion. While we employed buffers to induce this pattern change, it is conceivable that such dynamics could originate from other dynamical variables of cardiac  $\text{Ca}^{2+}$  cycling. In this case, our results point to more subtle dependencies in that the nonlinear dynamics of cardiac  $\text{Ca}^{2+}$  cycling can be easily disturbed into new dynamic regimes, potentially inducing a plethora of cardiac arrhythmias. It is therefore astonishing that cardiac  $\text{Ca}^{2+}$  dynamics more often than not behaves completely regularly; a fact that certainly deserves more attention.

We first reported the emergence of subcellular  $\text{Ca}^{2+}$  alternans via a saddle-node bifurcation in a PWL caricature of an established  $\text{Ca}^{2+}$  cycling model [15]. One might wonder if this novel form of subcellular  $\text{Ca}^{2+}$  alternans is a consequence of the approximations used in the derivation of the PWL model. The results presented here show that this is not the case. The fully nonlinear model exhibits the same instabilities. This provides further evidence that PWL models are valuable in exploring the behaviour of complex nonlinear systems and thus adds to earlier success stories such as the McKean model, which represents a PWL version of the Fitzugh-Nagumo model for the propagation of neural action potentials [57–59]. The advantage of PWL models is that the majority of the analysis can be performed semi-analytically, which greatly facilitates the exploration of the associated parameter space. In turn, this allows for a more comprehensive classification of the possible dynamics. In contrast, fully nonlinear systems can often only be dissected via direct numerical simulations, which is often only done for a small subset of parameter values. In this respect, PWL models can provide guidance for the analysis of the nonlinear systems and where to explore in parameter space for interesting behaviour.

The last point becomes especially pertinent for the exploration of the different spatial patterns that emerge via a saddle-node bifurcation. As Figs. 2, 3, 7 and 9 illustrate, the  $\text{Ca}^{2+}$  profiles across the network exhibit significant variability. In a PWL model, these patterns can be classified and understood from a linear stability analysis, which can be performed in closed form [15,16]. On the other hand, the nonlinear model requires direct simulations, which are computationally more expensive and limited in scope as to what parameter values to sample.

Our model is based on the Shiferaw-Karma model [34], which is purely deterministic. Due to the small number of RyRs and L-type  $\text{Ca}^{2+}$  channels per CRU, hybrid models have been developed in which  $\text{Ca}^{2+}$  diffusion between adjacent CRUs is deterministic, but the dynamics of RyRs and L-type  $\text{Ca}^{2+}$  channels are described by Markov chains, rendering their behaviour stochastic. These models have been very successful in explaining the emergence of subcellular  $\text{Ca}^{2+}$  alternans via e.g. the 3R theory or an order-disorder transition, where the latter makes contact with phase transitions in the Ising model for ferromagnetism [6,7,60,61]. An interesting questions therefore arises in how far results from a purely deterministic model can accurately describe the (patho)physiology of a fluctuation-driven biological system. This discussion is central to the study of intracellular  $\text{Ca}^{2+}$  dynamics. As a case in point, consider the ongoing debate on modelling  $\text{Ca}^{2+}$  dynamics mediated by the inositol-1,4,5-trisphosphate receptor [62–67]. The power of deterministic models is often seen in providing a baseline for comparison with stochastic/hybrid models. In other words, to fully appreciate the impact that molecular fluctuations have on emergent cellular dynamics, we need to ascertain how models behave in their absence. This philosophy guided us in the present study, and it will be an exciting avenue for future research to determine how stochastic gating dynamics of RyRs and L-type  $\text{Ca}^{2+}$  channels modulate the results reported here.

Our study explores the emergence of subcellular  $\text{Ca}^{2+}$  alternans in a ventricular myocyte with severely impaired cytosolic  $\text{Ca}^{2+}$  diffusion and where  $\text{Ca}^{2+}$  transport occurs mainly via the SR. This is reflected in the small coupling strengths  $\sigma_c = 2 \text{ s}^{-1}$  and  $\sigma_{\text{sr}} = 30 \text{ s}^{-1}$ , corresponding to diffusion time scales  $\tau_c = 500 \text{ ms}$  and  $\tau_{\text{sr}} = 33 \text{ ms}$ , respectively. To put these numbers into context, it is worth comparing them with diffusion time scales in healthy conditions. Care must be taken here

since reported diffusion coefficients vary greatly. For instance, Chen-Izu et al. [68] report cytosolic diffusion coefficients of  $150 \mu\text{m}^2 \text{s}^{-1}$  and  $300 \mu\text{m}^2 \text{s}^{-1}$  for transversal and longitudinal diffusion, respectively. For the SR, values of  $8 \mu\text{m}^2 \text{s}^{-1}$  and  $60 \mu\text{m}^2 \text{s}^{-1}$  have been reported. Since diffusive timescales scale as  $(\text{length scale})^2/\text{diffusivity}$ , we obtain values of 4ms (assuming a transverse separation of  $0.8 \mu\text{m}$ ) and 10.8 ms (assuming a longitudinal separation of  $1.8 \mu\text{m}$ ) for the cytosol. For the SR, we arrive at 40.5ms and 5.4ms if we use a longitudinal distance of  $1.8 \mu\text{m}$ . Restrepo et al. [42] point out that these estimates are crude and need to be refined. Based on this, they use diffusive coupling strengths of around 3 ms in the cytosol, but for the nonjunctional SR, values of 24 ms (longitudinal) and 7 ms (transverse) are used.

As stated above, our focus here is on tubulated myocytes. However,  $\text{Ca}^{2+}$  alternans have also been observed in non-tubulated cells such as atrial myocytes and failing ventricular myocytes [69–75]. In these cells, L-type  $\text{Ca}^{2+}$  channels are only located at the cell periphery, where they trigger  $\text{Ca}^{2+}$  release from the SR through the RyR. A  $\text{Ca}^{2+}$  wave then propagates centripetally from the periphery via diffusion and  $\text{Ca}^{2+}$  induced  $\text{Ca}^{2+}$  release [76,77]. Conceptually, it therefore makes sense to distinguish junctional CRUs (that contain L-type  $\text{Ca}^{2+}$  channels) and non-junctional CRUs (that lack L-type  $\text{Ca}^{2+}$  channels). Due to the stronger reliance on  $\text{Ca}^{2+}$  diffusion, it will be interesting to explore how differences in the diffusive coupling between CRUs and the fact there are two classes of CRUs shape subcellular  $\text{Ca}^{2+}$  alternans and whether the bifurcation structure observed for tubulated myocytes carries over to non-tubulated ones. Answering this question will not only unravel further similarities or differences between tubulated and non-tubulated myocytes, it will also advance our understanding of atrial fibrillation, which is projected to become epidemic with an ageing population [78].

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