communications physics

ARTICLE

Check for updates

1

https://doi.org/10.1038/s42005-023-01410-x

OPEN

Single-ended recovery of optical fiber transmission matrices using neural networks

Yijie Zheng ¹, Terry Wright¹, Zhong Wen^{2,3}, Qing Yang^{2,3} & George S. D. Gordon ^{1⊠}

Ultra-thin multimode optical fiber imaging promises next-generation medical endoscopes reaching high image resolution for deep tissues. However, current technology suffers from severe optical distortion, as the fiber's calibration is sensitive to bending and temperature and thus requires in vivo re-measurement with access to a single end only. We present a neural network (NN)-based approach to reconstruct the fiber's transmission matrix (TM) based on multi-wavelength reflection-mode measurements. We train two different NN architectures via a custom loss function insensitive to global phase-degeneracy: a fully connected NN and convolutional U-Net. We reconstruct the 64×64 complex-valued fiber TMs through a simulated single-ended optical fiber with $\leq 4\%$ error and cross-validate on experimentally measured TMs, demonstrating both wide-field and confocal scanning image reconstruction with small error. Our TM recovery approach is 4500 times faster, is more robust to fiber perturbation during characterization, and operates with non-square TMs.

¹ Optics and Photonics Research Group, Faculty of Engineering, University of Nottingham, Nottingham, UK. ² State Key Laboratory of Extreme Photonics and Instrumentation, College of Optical Science and Engineering International Research Center for Advanced Photonics, Zhejiang University, Hangzhou, China. ³ Research Center for Humanoid Sensing, Zhejiang Lab, Hangzhou, China. [™]email: george.gordon@nottingham.ac.uk

ltra-thin endoscopes are a promising technique for enabling cell-scale imaging in difficult-to-reach parts of the body, with the potential to improve disease detection in organs such as the pancreas and ovaries. Commercial products using imaging fiber bundles around 1mm in diameter are used in bile ducts and flexible and full-color imaging has been demonstrated using distal scanning mechanisms that are typically \sim 2 mm in diameter²⁻⁴. To further reduce the size of endoscopes, recent work has focused on imaging through ultra-thin multimode fibers with diameters of 0.125 mm and has achieved in vivo fluorescence imaging in brains of immobilized mice⁵. However, there are some key limitations of these imaging systems that use ultra-thin optical fiber. First, the thinnest such imaging devices are made using multimode fiber (MMF), which suffers from optical distortion that changes whenever the fiber is perturbed, particularly for longer fibers (>1m) required to reach deep inside the human body⁶. Second, to calibrate this distortion, practical endoscopes made using MMF or some types of fiber bundle require measurement of their transmission matrix (TM) which requires transmitting a set of well-defined modes of light from the proximal facet to the distal facet where the resulting optical field must be measured. If calibration is required immediately before use (e.g. for in vivo use), such components would be required on the distal tip and would thus compromise the ultra-thin form

A number of methods have been proposed to calibrate fiber TMs without distal access including guidestars^{8–10}, beacons that can be tracked^{11,12}, or reflective structures on the fiber tips^{7,13,14}. Gordon et al.¹⁴ proposed a single-ended method of TM recovery based on the fiber system shown in Fig. 1, with a specially designed reflector stack that provides different reflectances at different wavelengths. This approach avoids the need for measurement at both proximal and distal end of the fiber and works

for non-unitary TMs. The reflection matrix, $\mathbf{C}_{\lambda} \in \mathbb{C}^{M^2 \times M^2}$, where images are assumed to be $M \times M$ pixels, describes how an incident field $\mathbf{E}_{in} \in \mathbb{C}^{M^2}$ is transformed via propagation through the optical fiber, reflected by the reflector stack and finally transferred back through the fiber into an output field $\mathbf{E}_{out} \in \mathbb{C}^{M^2}$ at a wavelength of λ :

$$C_{\lambda}E_{in\lambda} = E_{out\lambda} \tag{1}$$

The reflectance matrix, $\mathbf{C}_{\lambda} \in \mathbb{C}^{M^2 \times M^2}$, is obtained from a forward pass via the TM, $\mathbf{A}_{\lambda} \in \mathbb{C}^{M^2 \times M^2}$, reflection via the reflector stack, $\mathbf{R}_{\lambda} \in \mathbb{C}^{M^2 \times M^2}$, and then a return pass via the TM, $\mathbf{A}_{\lambda}^{\top} \in \mathbb{C}^{M^2 \times M^2}$. It has been previously been shown that the forward TM at wavelength λ , \mathbf{A}_{λ} , can be unambiguously reconstructed based on the measured reflection matrices at 3 different wavelengths, with imaging performed at a fourth wavelength 14. This requires design of a special reflector stack whose reflection matrix changes with wavelength at a significantly faster rate than the fire TM, which may be achieved by alternately stacking metasurface reflectors with long-pass filters. A first-order dispersion model is assumed for the TM and has been experimentally validated to be >70% accurate over a 5 nm bandwidth for a 1–2 m length MMF using 110 modes, avoiding degeneracies arising from matrix logarithms 14, although recent work has shown MMF dispersion modeling over a much greater bandwidth 15. This leads to a set of 3 non-linear quadratic-form equations:

$$\mathbf{C}_{\lambda_1} = \mathbf{A}_{\lambda_1}^T \mathbf{R}_{\lambda_1} \mathbf{A}_{\lambda_1} \tag{2}$$

$$\mathbf{C}_{\lambda_2} = \left(e^{(\log \mathbf{A}_{\lambda_1} \frac{\lambda_1}{\lambda_2})}\right)^T \mathbf{R}_{\lambda_2} \left(e^{(\log \mathbf{A}_{\lambda_1} \frac{\lambda_1}{\lambda_2})}\right) \tag{3}$$

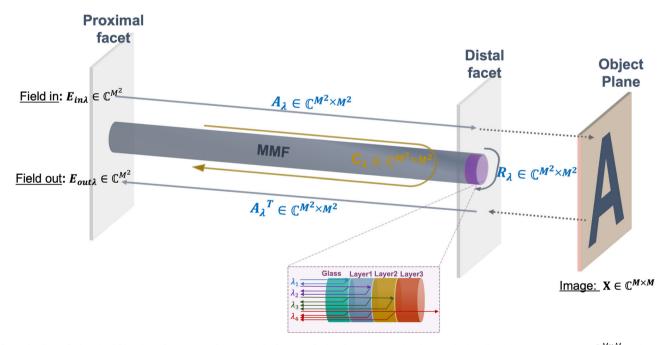


Fig. 1 Single-ended optical fiber imaging system for transmission matrix (TM) recovery. The object, which will produce an image $\mathbf{X} \in \mathbb{C}^{M \times M}$ is placed at the distal facet. Light with a field of $\mathbf{E_{in}} \in \mathbb{C}^{M^2}$ propagates from the proximal facet through the optical fiber, with the forward TM of the optical fiber defined as $\mathbf{A}_{\lambda} \in \mathbb{C}^{M^2 \times M^2}$ at the wavelength, λ . A reflector stack with a three-layer structure is placed at the distal facet, producing a reflector matrix $\mathbf{R}_{\lambda} \in \mathbb{C}^{M^2 \times M^2}$ at the wavelength λ . There are four different wavelengths used, where wavelengths λ_1 , λ_2 , and λ_3 are used for characterization and λ_4 for imaging. For each wavelength, light propagates through one or more layers of the stack and is partially reflected by metasurfaces at the interfaces between layers. This produces distinct reflector matrices at each wavelength, $R_{\lambda_{1.3}}$, which can be addressed using a tuneable laser. At wavelength λ_4 light passes fully through the stack so that imaging can be performed. Faithful image reconstruction require correction for the TM of the reflector stack using pre-calibrated values at this wavelength¹⁴. Reflection matrices, $\mathbf{C}_{\lambda} \in \mathbb{C}^{M^2 \times M^2}$, can be measured at relevant wavelengths to recover the TM.

$$\mathbf{C}_{\lambda_3} = \left(e^{(\log \mathbf{A}_{\lambda_1} \frac{\lambda_1}{\lambda_3})}\right)^T \mathbf{R}_{\lambda_3} \left(e^{(\log \mathbf{A}_{\lambda_1} \frac{\lambda_1}{\lambda_3})}\right) \tag{4}$$

where $e^{(\log A_{\lambda_1} \frac{\lambda_1}{\lambda_2})}$ is the TM adjusted for a wavelength λ_2 .

Currently, these equations are solved by using an iterative approach which relies on optimization of the entire TM¹⁴. This therefore scales in complexity with the square of the matrix dimension, incurring significant computational time, especially for large matrices. In practice, the TM shows high sensitivity to bending and temperature so in a practical usage scenario would need to be measured very frequently and reconstructed immediately prior to imaging. Large computational times are therefore not practical.

Considering this, there are several methods that have been developed in order to reduce the computational time for fiber imaging. These methods typically exploit prior knowledge about the fibers to improve or speed up TM reconstruction. For example, Li et al.¹⁶ proposed a compressed sampling method based on the optical TM to reconstruct full-size TM of a multimode fiber supporting 754 modes at compression ratios down to 5% with good fidelity. Similarly, look-up tables can be used with a reflective beacon for high-speed TM estimation over an experimentally sampled prior space¹². Huang et al.¹⁷ retrieved the optical TM of a multimode fiber using the extended Kalman filter, enabling faster reconstruction.

Recently, there has been work on using deep learning approaches, involving convolutional neural networks, to reconstruct images via multimode fibers both in transmission and reflection modes 18–20. These methods have the advantage of being fast, and also learning and utilizing prior information about the fiber properties and the objects being imaged. However, their performance typically degrades significantly under fiber perturbation because they do not have access to reflection calibration measurements required to unambiguously resolve a TM. Further, because such approaches seek to approximate the forward propagation of light and often only consider amplitude image recovery, they often rely on classical mean-squared error loss functions for training.

In order to incorporate reflection calibration measurements following fiber perturbation, it may instead be advantageous to use AI approaches to reconstruct a TM rather than an image, though there has been relatively little work in this area. When reconstructing a TM comprising complex numbers, a particular type of degeneracy arises that is not well handled by conventional AI loss functions: a global phase factor. In many physical problems, including the recovery of TMs for the purposes of image reconstruction and phase-hologram generation, global phase factors are not relevant as they do not affect the perceived performance of the system: it is the *relative* phase between pixels that must be preserved. The relative phase between rows or columns of fiber TMs or reflection matrices is typically preserved using a reference beam e.g. interferometry²¹ or referencing to a fiber mode²². Global phase may have a physical interpretation related to the physical length of the fiber, but in practice it is often arbitrary unless great care is taken. For example, in interferometric systems the global phase is likely to be arbitrary unless the optical path lengths of the reference and sample arms are perfectly matched, which is very challenging for multimode fibers. Further, the global phase often drifts during practical experiments²¹, and approaches using phase-retrieval produce entirely arbitrary global phase values²². Therefore, in many practical situations, conventional loss functions will convert arbitrary shifts in the global phase to large changes in loss, which can confound minimization algorithms used to fit AI models and cause overfitting.

In this paper, we therefore present a method of implementing single-ended recovery of an optical fiber TM by solving Eqs. (2)-(4) based on three reflection matrix measurements at three different wavelengths. Specifically, we present two different neural network architectures, fully-connected neural network (FCNN) and convolutional U-net-based neural networks, and demonstrate the performance of both. As a necessary step, we account for the global phase factor of the entire TM by developing a custom global phase insensitive loss function that avoids degeneracies introduced by conventional loss functions such as mean-squared error (MSE). We first validate our model by recovering 64 × 64 complex-valued fiber TMs through a simulated single-ended optical fiber system (shown in Fig. 1) with ≤4% error for both FCNN and convolutional U-net architectures. We then demonstrate image reconstruction through fiber based on recovered TMs for two different imaging modalities: widefield imaging, achieving ≤9% error, and confocal imaging, achieving ≤5% error. We highlight several advantages of this TM recovery approach compared to previous TM recovery methods. Firstly, once the model is trained (~100 h), it only requires ~1 s for reconstruction, which is 4500 times faster than pre-existing iterative approaches. Secondly, the conventional method¹⁴ can only reconstruct square TM cases, whereas this method is compatible with non-squareshaped TM with ≤8% error, useful for many practical cases where optical systems may have different mode bases at proximal and distal ends. Third, the requirements for the reflectors in terms of matrix properties are related and then can have arbitrary distributions of eigenvalues.

Results

Simulated TM recovery. This TM recovery model was trained on a simulated dataset comprising 900,000 sets of simulated reflection matrices, C_{λ} at 3 wavelengths, $\lambda_1 = 850$ nm, $\lambda_2 = 852$ nm and $\lambda_3 = 854$ nm, as input and a complex-valued non-unitary TM at wavelength λ_1 , \mathbf{A}_{λ_1} as output. Performance was monitored during training using 200,000 validation data that were not used in training. Final performance figures for the model were evaluated using an additional 100,000 data that were not part of the validation set. Figure 2(a) shows the training and validation loss in training the FCNN model over 2500 epochs using different loss functions, namely conventional mean absolute error (MAE), and our globalphase insensitive custom loss function (Eq. (11)). Our global-phase insensitive loss functions show a decreasing loss in both training (yellow line) and validation (purple line) in the first 2000 epochs and convergence after 2500 epochs, whereas the MAE loss function exhibits fluctuating non-converging loss values for both training (blue line) and validation (red line). An example of a reconstructed TM predicted by the FCNN model at different epochs is shown inset in Fig. 2a. It can be seen that the predicted TM approaches the target TM from 300 epochs to 2500 epochs, enabled by the custom loss function. Figure 2b compares the TM result predicted by our two different neural network architectures using different loss functions. Both FCNN and convolutional U-net-based neural networks cannot recover TM when using the MAE loss function but are capable of recovering TM using the global phase insensitive loss function, with an average loss (metric defined in Eq. (8)) of ≤4% over 100,000 test TMs. Compared to the previous iterative approach, which requires nearly 10 hours to converge with an average loss of ≤0.5%, our method shows a larger ≤4% average loss, but images retain acceptable visual quality of reconstructed images (shown in "Result" section "Widefield image reconstruction based on recovered TM"). Furthermore, we also evaluated the computational resource usage of the two different neural network architectures as shown in Fig. 2c. Training was implemented using Tensorflow 2.0 running on an NVIDIA Tesla V100 GPU. Compared to FCNN, the convolutional

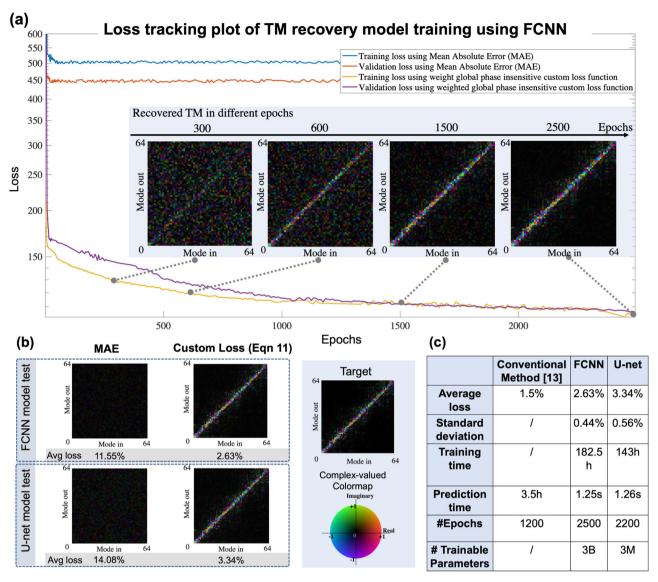


Fig. 2 Simulated TMs recovered by training Neural Network (NN) models. a Training and validation loss tracking plot using MAE and custom loss function (Eq. (11)) of fully-connected neural network (FCNN) model. Blue and red line represent training and validation loss using mean absolute error (MAE) loss function. Yellow and purple line represent training and validation loss using our global-phase insensitive loss function. TM recovery results over different epochs are shown inset. b TM recovery results using two different neural network architectures (i.e. FCNN and convolutional U-net networks), with two different loss functions, namely MAE and custom loss function in Eq. (11). c Comparison between FCNN and convolutional U-net architecture in aspects of average loss, standard deviation, training time, prediction time, number of converging epochs and number of trainable parameters. In complex-valued colormap, hue represents phase and lightness/darkness represents amplitude.

U-net shows significant advantages in memory usage, requiring 1000 times fewer trainable parameters, and in convergence time, which is reduced by 20%. However, it shows 0.7% larger average loss on the test set. Both FCNN and convolutional U-net can recover TM at a loss $\leq 4\%$ (standard deviation 0.44% and 0.56% respectively), with ~ 1 s prediction time.

Widefield image reconstruction based on recovered TM. Next, we examine a widefield imaging modality to evaluate the performance of recovered TMs at a fourth wavelength (the imaging wavelength), $\lambda_4=854.5$ nm, where we assume a pixel basis at the fiber output. We considered three example images denoted $\mathbf{x} \in \mathbb{C}^{8\times 8}$: an amplitude-only image with a 'space invader' pattern, a phase-only digit with a uniform amplitude and a random complex-valued image. Random noise was added to better simulate expected behavior in a real system (shown in Eq. (7)).

Figure 3 shows the image reconstruction results based on recovered TM using FCNN and convolutional U-net networks. It can be seen that all three images can be successfully reconstructed based on recovered TMs using both neural network models. Using the IMMAE (image MAE metric defined in Eq. (9)) we achieved error ≤9% and using SSIM (structural similarity index measure metric defined in Eq. (10) we achieve similarity ≥83%. Because of the superior error performance of the FCNN approach, for the remainder of this work we choose this model to demonstrate proof-of-principle performance of neural network TM recovery under a range of realistic scenarios. However, when scaling to larger size TMs, the convolutional U-net may be more favorable due to fewer trainable parameters.

Effect of fiber perturbation widefield image reconstruction. We then evaluate the robustness of our TM recovery model by

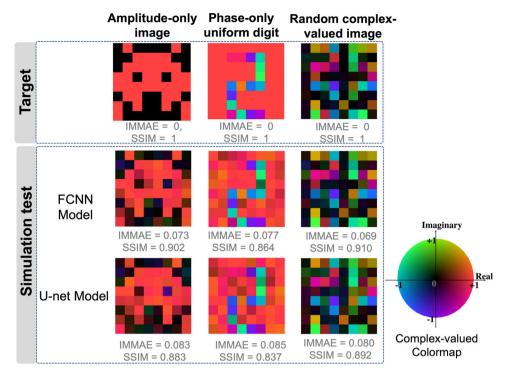


Fig. 3 Widefield image reconstruction based on recovered transmission matrices (TMs) using fully-connected neural network (FCNN) and convolutional U-net networks. We considered three example images: an amplitude-only image with a `space invader' pattern, a phase-only digit with a uniform amplitude and a random complex-valued image. Two metrics are defined to evaluate the image reconstruction performance, namely image mean absolute error, IMMAE (Eq. (9)) and structural similarity index measure, SSIM (Eq. (10)). In complex-valued colormap, hue represents phase and lightness/darkness represents amplitude.

simulating the effect of the TM changing mid-way through fiber characterization. Specifically, we simulate a situation in which the reflection matrices measured at the first two wavelengths (C1 and C₂) are recorded using a fixed TM, but the reflection matrix measured at the third wavelength C₃ is recorded initially using this same TM but the final few columns are generated using a different TM. Therefore, we simulated 10 sets of 64×64 reflection matrices with five different perturbation rates indicating the numbers of columns swapped (2/64, 4/64, 8/64, 16/64, and 32/64). Figure 4 shows the results of recovering the TM based on these perturbed measurements, and then using this perturbed TM estimate to perform widefield image reconstructions. This is repeated for different fiber perturbation rates based on our pre-trained TM recovery FCNN model. It can be seen that our TM recovery model is compatible with optical fibers with a small perturbation rate (below 6%) with TM average loss ≤8% (standard deviation $\leq 0.82\%$), IMMAE $\leq 19\%$ and SSIM $\geq 76\%$ but performance degrades above this.

Confocal image reconstruction based on recovered TM. Many fiber imaging systems use a confocal imaging approach, rather than widefield, because of its superior resolution. We therefore simulated confocal scanning imaging reconstruction through our recovered TM. For this, we used a simulated LP basis based on a typical fiber profile (see "Methods" section). We addressed 128×128 spot positions and found the average percentage of power in the focus to be 48.5% using recovered TM, which compares favorably to that achieved using an identity matrix as the TM (49.9%) as shown in Fig. 5a. Next, we reconstructed confocal images of three target images, denoted $\mathbf{x} \in \mathbb{C}^{128 \times 128}$ that contain the same pattern shown in "Result" section "Widefield image reconstruction based on recovered TM" by integrating total reflected power for each spot position. We used $\lambda_4 = 845.5$ nm

here for imaging. Figure 5b-d shows the confocal image results using FCNN model. It can be seen that all three types of confocal images can be successfully reconstructed based on recovered TMs, with IMMAE ≤5% and SSIM ≥90%. Also, it shows 3% points less image error and 4% points higher similarity between reconstructed and target confocal images compared to widefield imaging.

Non-square TM recovery. We next examine the practical case of non-square TMs, e.g. where the desired representation at the distal end of a fiber might be different from that used at the proximal end and may have more elements. This might be the case, for example, when measuring forward TMs to use to train such a network. To recover a TM $\mathbf{A} \in \mathbb{C}^{M_d \times M_p}$, we require that the reflection matrix, $\mathbf{C} \in \mathbb{C}^{M_p \times M_p}$ and that the reflector matrix, $\mathbf{R} \in \mathbb{C}^{M_d \times M_d}$. M_p and M_d represent the number of elements used for the basis representation at the proximal and distal ends of the fiber respectively. Figure 6 shows one example of recovered non-square-shaped $\mathrm{TM} \in \mathbb{C}^{6 \times 12}$ using FCNN, with the average loss of 3.96% (standard deviation 0.38%). 'Wide' TMs (with $M_d < M_p$) may be over-constrained by larger dimension C producing stable solutions, while 'tall' TMs (with $M_p < M_d$) may be underconstrained producing degenerate solutions.

Reflector matrix conditioning. Explicit conditions on the reflector matrices, **R**, namely having distinct eigenvalues, have been a requirement in previous approaches^{7, 14}. Here, we test our TM recovery FCNN model with different reflector matrix conditioning by varying the number of distinct eigenvalues, as shown in Supplementary Figure 1. We examined the recovered TMs for 3 conditionings of **R**: 1 distinct eigenvalue (unitary, all eigenvalues the same), 2 distinct eigenvalues, and 6 distinct eigenvalues. The average recovery loss achieved is 5.02% (standard deviation

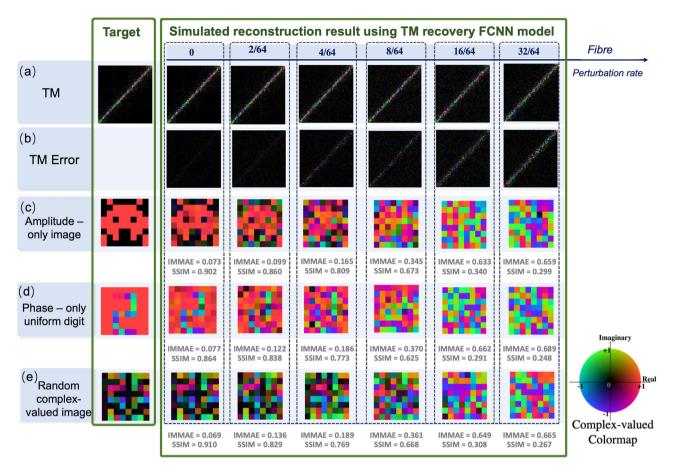


Fig. 4 Effect of simulated perturbations of fiber transmission matrices (TMs) during reflection-mode characterization. Perturbations are simulated by swapping columns between two different TMs at wavelength λ_3 . Two metrics are defined to evaluate the image reconstruction performance based on recovered TM using fully-connected neural network (FCNN), namely image mean absolute error, IMMAE (Eq. (9)) and structural similarity index measure, SSIM (Eq. (10)). **a** Estimated perturbed TM. **b** Error in estimated TM. **c** Image reconstruction of amplitude-only target (uniform phase) using estimated perturbed TM. **d** Image reconstruction of phase-only target (uniform amplitude) using estimated perturbed TM. **e** Image reconstruction of complex amplitude and phase target using estimated perturbed TM.In complex-valued colormap, hue represents phase and lightness/darkness represents amplitude.

0.43%), 4.96% (standard deviation 0.41%), 3.88% (standard deviation 0.37%) respectively, demonstrating that the recovery process is compatible with various reflector matrices conditions.

Computational resource usage. As the dimension of recovered images increases, we expect an increase in the TM dimension thus requiring more computational resources. Empirically measured computational resources are plotted in log-scale in Fig. 7a-c: minimum training data, minimum memory usage, and converging time respectively. All indicate a quadratic relationship to the image dimension M for both FCNN and convolutional U-net models. For practical imaging applications we would desire at least 32 × 32 image resolution, giving a 1024 × 1024 TM, which would require training with >10 million examples, leading to memory consumption >1.5TB for the FCNN. By comparison, the convolutional U-net would require only 1.1TB of memory consumption. Compared to FCNN, convolutional U-net shows potential advantages in using 25% fewer memory resources and 20% less training data within 15% less training time. Figure 7d compares the prediction time using our neural network model with the conventional methods using iterative optimization approaches¹⁴, where our FCNN model shows less reconstruction time (\sim 1s vs. 1920s for a 12 \times 12 TM).

Validation with experimental TMs. Finally, to demonstrate applicability to practical systems we cross validated our model on experimentally measured TMs recorded under a representative range of likely fiber conformations¹². The graph of loss vs. epoch for the different training steps used to adapt the model pretrained on simulated data is shown in Supplementary Figure 2. The model is first re-trained from step 1 with additional inputs using random matrices to avoid overfitting to the prior distribution of simulated matrices (step 2). We next continued training the model on a small subset of the experimental data to aid domain transferability (step 3). By creating 'submatrices' we are effectively implementing a downsampling basis change and so expect some change in correlations betweens TM elements. However, by including random matrices in our training set we actively prevent the model from learning a strong prior distribution over these correlations and thus overfitting.

The final model achieves recovery of simulated TMs with an average loss of 3.38% (standard deviation 0.48%) and experimental matrices with 3.42% (standard deviation 0.57%), suggesting that it is applicable to realistic fiber TMs under various conformations. An example of experimental TM used for the test at each step is shown inset in Supplementary Figure 2, where the predicted TM is getting closer to the target TM from step 1 to step 3.

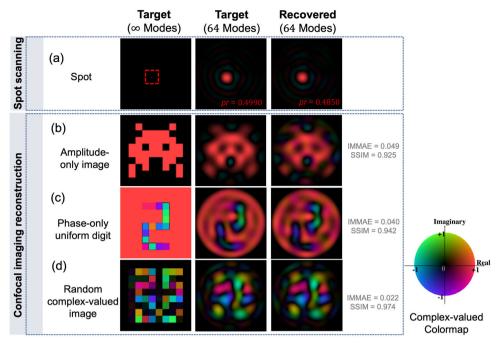


Fig. 5 Spot scanning and confocal image reconstruction based on recovered transmission matrices (TMs) using fully-connected neural network (FCNN) model. The spot and 2D full samples are generated using 128 × 128 targets. Power ratio (*pr*) is defined to calculate the average percentage of power in the focus by scanning 128 × 128 approximate spot positions. Two metrics are defined to evaluate the image reconstruction performance, namely image mean absolute error, IMMAE (Eq. (9)) and structural similarity index measure, SSIM (Eq. (10)). **a** Creation of a focussed spot in perfect scenario and band-limited scenario with 64 modes using both actual (target) and recovered TMs. **b** Image reconstruction using confocal scanning for amplitude-only image, (**c**) phase-only image and (**d**) random complex valued image.In complex-valued colormap, hue represents phase and lightness/darkness represents amplitude.

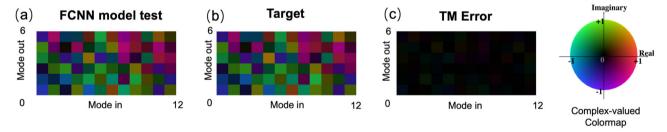


Fig. 6 Non-square shaped transmission matrix (TM) \in $C^{6 \times 12}$ recovered by our TM recovery model using fully-connected neural network (FCNN) architecture. a TM recovered by FCNN model. b Target TM. c Error between recovered and target TMs. In complex-valued colormap, hue represents phase and lightness/darkness represents amplitude.

Discussion

We have demonstrated the successful reconstruction of forward fiber TMs based on reflection-mode measurements at multiple wavelengths using a neural network-based approach encompassing two architectures: a fully-connected neural network and a convolutional U-Net. Previous work applying neural networks to fibers has focussed on image reconstruction as the end goal, but we instead focus on TM reconstruction. Such an approach is more flexible as the inputs to the network are calibration measurements that reflect a fiber's deformation state at any given time – previous image reconstruction approaches have instead learned a static representation of the fiber TM encoded in the neural network weights. Using our approach, the recovered TM will be accurate up to the most recent calibration measurements and can be used for high-speed image recovery via conventional matrix operations.

One major challenge of recovering the TM is the presence of degenerate global phase shift. Previous work on image reconstruction has addressed this problem by training separate

networks for amplitude and phase recovery in purely real space and accepting relatively poor performance for phase recovery¹⁸. Here, we present a loss function that is insensitive to this global phase degeneracy and show a high degree of convergence compared to conventional MAE metrics. We believe this metric could also find applications in neural network-based computer-generated holography or phase retrieval.

There are several major advantages to our neural network approach compared to previous iterative approaches¹⁴. First, the prediction time is very fast (typically ~1s), over 4500x faster than the existing iterative approach, which makes this a feasible approach for future real-time imaging, Training the network is much slower, but this only need to be done once per fiber for a fixed reflector as a one-off calibration step. Second, our approach shows robustness to the fiber TM changing part way through characterization measurements, as is likely to happen during real in vivo usage, and can tolerate up to 6% column swaps between different reflection matrices. This performance could be further improved by re-training the network with perturbed examples as

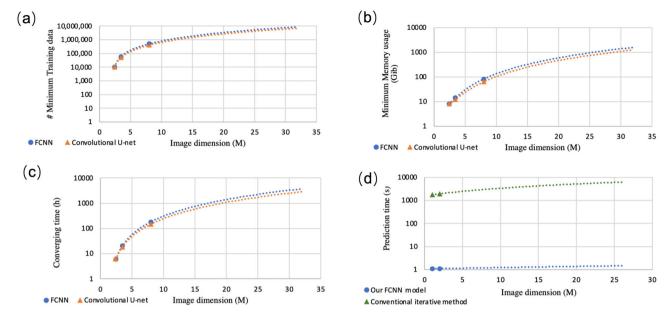


Fig. 7 Empirically measured computational resources plotted in log-scale. a Minimum training data versus the number of image dimensions, plotting in log-scale. b Minimum memory usage versus the number of image dimensions, plotting in log-scale. c Converging time versus the number of image dimensions. d Prediction time of using our transmission matrix (TM) recovery model and conventional method, plotting in log-scale.

input, allowing it to learn an 'error correction' strategy. Third, the approach can reconstruct non-square TMs. This is important because the sampling basis of the light on the proximal facet is often the pixel basis of the camera but at the distal end it may be a mode basis of the fiber (e.g. LP modes). The fiber may support many fewer modes than the camera has pixels. Therefore, to optimize speed and imaging performance it is often desirable to retrieve a TM in the mode basis of the fiber that can easily be addressed using our camera coordinates: hence a non-square TM. Finally, our recovery process is compatible with various reflector matrices conditions whereas in previous models the eigenvalues are required to be distinct^{7,14}. However, it is noted that eigenvalues are unlikely to be identical in any experimental system due to small mode-dependent power losses, but the removal of this condition may increase robustness to noise.

Several trade-offs should be considered when using this approach. The first trade-off is the need for large amounts of experimental transmission and reflection measurements to train the network. This can be addressed by augmenting experimental data with large amount of simulated fiber data: we have previously found good agreement between simulated and experimental matrices 14. To implement these simulations, the reflector matrices would need to be known in advance e.g. by performing TM measurements of a fiber, attaching a reflector, then measuring reflection matrix with minimal fiber perturbation. Alternatively, it may be possible to devise a method of reliably manufacturing reflectors with consistent and highly reproducible properties. Our simulations assume limited fiber bandwidth to avoid degeneracies arising from matrix logarithms, but this bandwidth could be extended using a non-linear model of the fiber TM over a much broader wavelength range 15. This joint simulation-experiment approach borrows ideas from data augmentation and domain transfer²³⁻²⁵. The use of adaptive loss functions, such as in generative-adversarial networks, may further enable convergence using relatively small experimental datasets, or else help to generate further training data. In these latter scenarios it could be envisioned that the reflector need not be characterized in advanced and can be inferred from a small number of experimental measurements.

The second key trade-off is that the training process is very memory-intensive for dealing with large sizes of TM that are

typically encountered in imaging applications e.g. 1024×1024 would require over 1TB for training the recovery model. The convolutional U-net architecture has much (×1000) fewer trainable parameters, which reduces memory usage somewhat, although the large dimension of each input TM also has a large influence on the memory usage. However, using convolutional architectures may come at the expense of slightly increased error (a few percent) as we observed in our TM reconstruction results. One possible solution is to develop matrix compression techniques such as auto-encoder models to represent matrices in a low-dimensional latent space. Reducing batch size will also reduce memory usage but can lead to greater fluctuations and poorer convergence.

We anticipate this neural network-based TM recovery model will lead to machine-learning models for complex-valued data, for example in holographic imaging and projection and phase retrieval, where both phase control and speed are required.

Conclusions

Overall, our model for reconstructing 64×64 complex-valued fiber TMs through a single-ended optical fiber system achieves $\leq 4\%$ error for both FCNN and convolutional U-net-based neural network architectures. By re-training our FCNN model we also show that it can reconstruct experimentally measured 64×64 TMs with 3.42% error. Using our recovered TMs we demonstrate image reconstruction of complex objects in two imaging modalities: 8×8 pixel widefield imaging, achieving IMMAE $\leq 9\%$ and SSIM $\geq 83\%$, and confocal scanning, achieving 48.5% power focused in the spot and $\leq 5\%$ IMMAE and $\geq 90\%$ SSIM.

Methods

Simulated data generation. We present a TM recovery method that uses neural networks, instead of using iterative approaches ¹⁴, to solve the Eqs. (2)–(4). Figure 8 shows the schematic of this TM recovery model. Specifically, we first simulated N optical fiber TMs, $\mathbf{A}_{\lambda_1} \in \mathbb{C}^{M^2 \times M^2}$, at a wavelength of λ_1 as the ground truth. Here we use M=8 and $\lambda_1=850$ nm. Our simulation model aims to recreate typical properties found in practical fiber TMs. First, we assume that TMs are sparse in some commonly used basis e.g.

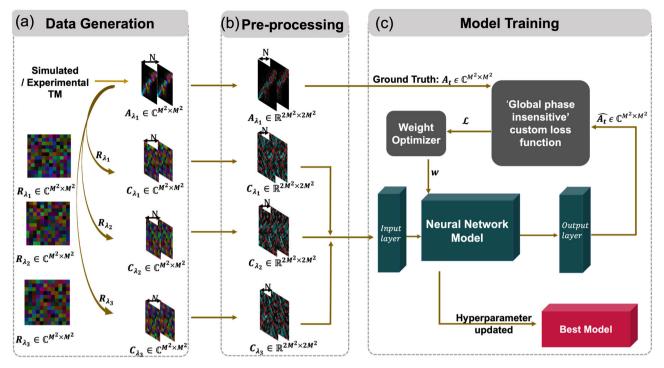


Fig. 8 Schematic of transmission matrix (TM) recovery model. This contains (**a**) data generation, (**b**) data pre-processing, and (**c**) model training. *N* pairs of TM are firstly simulated as the ground truth. λ_1 , λ_2 , and λ_3 represent three different wavelengths (in our case, 850 nm, 852 nm and 854 nm). The input of the model is all real-valued matrices concatenated with reflection matrices at three different wavelengths. *L* represents custom loss function and *w* represents the weight updated by the optimizer.

LP modes for multimode fibers or pixel basis for multicore fibers²⁶. Second, we assume TMs can be arranged such that the majority of power intensity lies along the main diagonal with additional power spread along sub-diagonals, which is also typically observed when using bases closely matched to the fiber eigenbasis²⁷. Third, we assume that realistic TMs are slightly nonunitary, with mode-dependent loss values (i.e. condition numbers) in the range of 3-5^{26,27}. To meet these assumptions, we generate a uniformly distributed random tri-diagonal matrix, $\mathbf{B} \in \mathbb{C}^{64 \times 64}$, which has non-zero elements only at the main diagonal, subdiagonal and superdiagonal. We then compute the left singular matrix $\mathbf{U} \in \mathbb{C}^{64 \times 64}$ and right singular matrix $\mathbf{V} \in$ $\mathbb{C}^{64\times 64}$ via singular value decomposition (SVD). We then apply a new singular value distribution via a matrix $\mathbf{S}_{new} \in \mathbb{R}^{64 \times 64}$, a diagonal matrix that contains random values along its diagonal ranging from 0.5 to 2.5 to simulate our expected TM. We then construct the TM at λ_1 as:

$$\mathbf{A}_{\lambda} = \mathbf{U} * \mathbf{S}_{\text{new}} * \mathbf{V}^{T} \tag{5}$$

Next, we apply Eqs. (2)–(4) to simulate corresponding TMs, A_{λ_1} and A_{λ_1} at wavelengths $\lambda_2=852$ nm and $\lambda_3=854$ nm. Here, we use wavelengths $\lambda_1=850$ nm, $\lambda_2=852$ nm, and $\lambda_3=854$ nm as physically realistic values within the TM bandwidth of a typical endoscope length fiber (~2 m)¹⁴.

Following this, we simulate reflectors on the fiber distal tip by generating three complex-valued matrices with complex uniform randomly distributed elements (-1 to 1 and -i to i). These three matrices then form our reflector matrices, $\mathbf{R}_{\lambda_1} \in \mathbb{C}^{M^2 \times M^2}$, $\mathbf{R}_{\lambda_2} \in \mathbb{C}^{M^2 \times M^2}$, and $\mathbf{R}_{\lambda_3} \in \mathbb{C}^{M^2 \times M^2}$ at wavelengths λ_1 , λ_2 and λ_3 respectively. By generating reflectors in this way we ensure with high probability, according to random matrix theory, that the eigenvalues are distinct²⁸.

Finally, we combine the TMs and reflector matrices to generate N sets of complex-valued reflection matrices $\mathbf{C}_{\lambda_1} \in \mathbb{C}^{64 \times 64}$, $\mathbf{C}_{\lambda_2} \in \mathbb{C}^{64 \times 64}$, and $\mathbf{C}_{\lambda_3} \in \mathbb{C}^{64 \times 64}$ at three different wavelengths $\lambda_1 = 850$ nm, $\lambda_2 = 852$ nm and $\lambda_3 = 854$ nm.

To feed this data to our neural network, which only accepts real numbers, we convert inputs and outputs from complex to real-valued data. A 2×2 complex-valued matrix can be represented by a 4×4 real-valued matrix as follows²⁹:

$$\begin{bmatrix} a+bi & c+di \\ e+fi & g+hi \end{bmatrix} \mapsto \begin{bmatrix} a & -b & c & -d \\ b & a & d & c \\ e & -f & g & -h \\ f & e & h & g \end{bmatrix}$$
 (6)

where, \mapsto indicates an isomorphism.

Finally, the input of the model, three $C_{\lambda} \in \mathbb{C}^{128 \times 128}$ at different wavelengths are normalized using in the range from -1 and 1. Each set of 3 reflection matrices, $C_{\lambda_{1..3}}$ represents a single input to our neural network model. We split the N data into training, validation, and test sets with an 8:2:1 ratio. The validation set is expected to provide unbiased evaluations and stopping criteria on unseen data, and test set aims to examine the generalization performance of the model on unseen data. Test set is independent of the validation set and contains unseen data that is not used during training process. The model is trained with the ADAM optimizer using our custom-defined loss function. Python was used for model training and MATLAB was used for data preprocessing and post-processing because of its ease of use for complex matrix computations.

Imaging modalities. We validate our system via two commonly used fiber imaging modalities: wide-field and confocal scanning. For wide-field imaging we assume a pixel basis at the fiber distal end, and that a ground-truth complex image $\mathbf{X} \in \mathbb{C}^{M^2}$ passes via

the simulated optical fiber ground-truth TM at a fourth wavelength $\lambda_4=854.5$ nm. We then use the recovered TM at a fourth wavelength $\lambda_4=854.5$ nm to estimate original image and compare this to the ground-truth. For simplicity, we assume the object is located at the distal fiber facet with no loss coupling into and out of the fiber, and we neglect the loss in transferring through the reflector stack but consider random Gaussian noise to better simulate expected behavior in a real system. Theoretically, the reconstructed widefield image, $\hat{\mathbf{X}}_j \in \mathbb{C}^{M^2}$ can be calculated by:

$$\hat{\mathbf{X}}_{\mathbf{i}} = (\hat{\mathbf{A}}_{\lambda_i}^T)^{-1} (\mathbf{A}_{\lambda_i}^T \mathbf{X}_{\mathbf{i}} + \mathbf{Z})$$
 (7)

where, **Z** is random Gaussian noise with a power of 2% of the target signal. $\hat{\mathbf{X}}_j$ is the reconstructed image, \mathbf{X}_j is the target image, $\hat{\mathbf{A}}_{\lambda_4}$ and \mathbf{A}_{λ_4} are the recovered TM and target TM at wavelength λ_4 respectively.

For confocal imaging, which is commonly used in fiber imaging 30 , we assume an LP mode basis at the fiber output, which is a realistic and widely used fiber basis 31 . To implement this, we first simulated a multimode fiber with a core radius of 30 μm , length of 1.5 m and a numerical aperture (NA) of 0.24 and used 64 of the available modes as our basis for creating a spot to be scanned. We used our recovered TM to estimate the required proximal field to create a spot then examined the expected spot by forward propagating via the ground truth TM. We next scanned 128×128 approximate spot positions and found the average percentage of power within the FWHM of the spot. Using this approach we reconstructed confocal images of three target images, denoted $\mathbf{x}\in\mathbb{C}^{128\times128}$ that contain the same pattern shown in "Result" section "Widefield image reconstruction based on recovered TM" by integrating total reflected power for each spot position.

Metrics. We next define loss metrics to compare the complex overlap integral between the target and recovered results. However, due to the degenerate global phase factor, this complex overlap integral is multi-valued. Therefore, the loss metrics defined here first normalize to correct for the global phase term (see Methods Section Global phase insentive loss function) before calculating the complex correlation. This is an essential step to gauge the accuracy both for TM recovery and image reconstruction in widefield and confocal modalities.

To gauge the accuracy of our TM recovery we define an average loss metric by calculating the average mean absolute error (MAE) of each validated TM in the test data:

$$\text{average loss} (\hat{\mathbf{A}}_{\mathbf{t}}, \mathbf{A}_{\mathbf{t}}) = \frac{1}{N_{test}} \times \frac{1}{4M^2} \sum_{n=1}^{N_{test}} \sum_{t=1}^{4M^2} |\hat{\mathbf{A}}_{\mathbf{t}} - \mathbf{A}_{\mathbf{t}} e^{i\phi_c}| \qquad (8)$$

where, $\hat{\mathbf{A}}_t$ is the recovered TM, $\mathbf{A_t}$ is the target TM, $e^{i\phi_c}$ is the global phase normalization term, $4\,\mathrm{M}^2$ is the total number of TM elements, and N_{test} is the number of data used for testing.

To gauge the accuracy of widefield reconstructed image based on the recovered TM, we define two metrics, namely the image MAE (IMMAE) and complex-valued based structural similarity index measure (SSIM) of each reconstructed image:

IMMAE
$$(\hat{\mathbf{X}}_{j}, \mathbf{X}_{j}) = \frac{1}{M^{2}} \sum_{i=1}^{M^{2}} |\hat{\mathbf{X}}_{j} - \mathbf{X}_{j} e^{i\phi_{c}}|$$
 (9)

SSIM
$$(\hat{\mathbf{X}}_{j}, \mathbf{X}_{j}) = \frac{2|\sum_{j=1}^{M^{2}} \hat{\mathbf{X}}_{j} \mathbf{X}_{j}^{*} e^{i\phi_{c}}| + K}{\sum_{j=1}^{M} |\hat{\mathbf{X}}_{i}|^{2} + \sum_{j=1}^{M^{2}} |\mathbf{X}_{i}|^{2} + K}$$
 (10)

where, M^2 is the total number of pixels of image X_j , X_j^* is the complex conjugate of X_j , K = 0.03 is a positive constant to improve the robustness when the local signal to noise ratios are low. These two metrics can also be extended to evaluate the performance of recovered confocal images.

In the confocal case, we compare recovered images $\hat{\mathbf{Y}}$ against the confocal imaging scenario with an identity TM, \mathbf{Y} , using the two metrics (IMMAE and SSIM) introduced in Eqs. (9)–(10). This aims to do a fair comparison considering the effect of conversion between fiber mode basis and pixel basis.

Network architectures. We defined two neural network models: a fully-connected neural network (FCNN) and convolution U-netbased neural network as shown in Fig. 9. The FCNN is a ten-layer densely connected neural network (eight hidden layers), including 32,768 neurons in first and last hidden layers and 8192 neurons in other layers, all with Leaky ReLU activation function. Figure 9 shows the FCNN architecture, where derivation matrices $\mathbf{C}_{\lambda_1} \in \mathbb{R}^{128 \times 128}$, $\mathbf{C}_{\lambda_2} \in \mathbb{R}^{128 \times 128}$, $\mathbf{C}_{\lambda_3} \in \mathbb{R}^{128 \times 128}$ are flattened into 1D arrays and then concatenated as the input of the model (with the size of 49,152 × 1) and TM $\mathbf{A}_{\lambda_1} \in \mathbb{R}^{128 \times 128}$, flattened into 1D array as the output (with the size of $16,384 \times 1$). Batch normalization layers were defined between every dense layer and dropout layers at the rate of 0.2 were defined after the first two dense layers. Also two skip connections were developed in order to prevent the model overfitting. The model was trained iteratively with the global phase-insensitive custom loss function used. The training dataset for recovering 64 × 64 TM consisted of 500,000 matrices and the model was run for 2500 epochs, taking 182.5 hours using Tensorflow 2.0 running on a NVIDIA Tesla V100 GPU. The Adam optimizer was used with a learning rate of 0.004 in a decay rate of $1e^{-4}$.

Next, we developed a U-net-based model that used encoderdecoder architecture, including seven Conv2D and DeConv2D

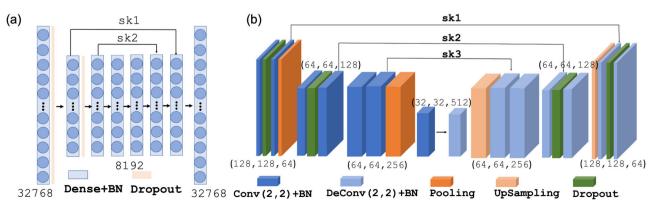


Fig. 9 Architectures of two different neural network models used for TM recovery. a Fully-connected neural network, (b) Convolutional U-net.

layers respectively and two MaxPooling and UpSampling layers respectively with LeakyRelu activation function in each layer. Figure 9 shows this architecture, where reflection matrices $\mathbf{C}_{\lambda_1} \in \mathbb{R}^{128 \times 128}, \ \mathbf{C}_{\lambda_2} \in \mathbb{R}^{128 \times 128}, \ \mathbf{C}_{\lambda_3} \in \mathbb{R}^{128 \times 128}$ are defined in three channels as the input of the model (with the size of $128 \times 128 \times 3$) and TM $\mathbf{A}_{\lambda_1} \in \mathbb{R}^{128 \times 128}$, as the output (with the size of $128 \times 128 \times 1$). Batch normalization layers were defined between every layer and dropout layers at the rate of 0.2 were defined after the second and last second Conv layers. Also three skip connections were developed in order to prevent the model being overfitted. The model was trained iteratively with the global phase insensitive custom loss function defined. Also, 2200 epochs were used for training 400,000 training datasets using 143 h. The Adam optimizer was used with a learning rate of 0.004 in a decay rate of 1e-4.

Global phase insensitive loss function. Widely used conventional loss functions such as mean absolute error (MAE) or mean squared error (MSE) calculate the absolute difference between predicted and target output values. However, there is a class of problems whose solutions trained by deep learning models are degenerate within a global phase factor, but whose relative phase between pixels must be preserved. This class includes problems where complex TMs are reconstructed and relative phase, but not global phase, could extend to phase-hologram generation algorithms where replay-field phase is relavant³². This is depicted visually in Supplementary Fig. 3a, which shows one example of a pair of predicted and target matrices with complex entries depicted as vectors. Supplementary Fig. 3b shows the complex error between these two matrices when using MAE as the loss function. Due to the global phase shift, we observe that the vectors have large magnitudes, which will lead to an overall very large MAE when their magnitudes are summed. In the limiting case (e.g. when the phase shift is of π) where the predicted and target matrices are identical, this global phase shift can result in a normalized MAE of 100% when the true value should be 0%. To avoid this problem, we propose a custom loss function termed a 'global phase insensitive' loss function that normalizes for this global phase factor:

$$L(\widehat{\mathbf{A}}_{\mathbf{t}}(w), \mathbf{A}_{\mathbf{t}}) = \sum_{t=1}^{4M^2} \left| \widehat{\mathbf{A}}_{\mathbf{t}}(w) - \mathbf{A}_{\mathbf{t}} e^{i\phi \left(\operatorname{Tr}(\mathbf{A}_{\mathbf{t}}^H \widehat{\mathbf{A}}_{\mathbf{t}}(w)) \right)} \right| + \frac{\alpha}{2} \|w\|^2$$
 (11)

where, $\widehat{\mathbf{A}_t}(w) \in \mathbb{C}^{M^2 \times M^2}$ and $\mathbf{A_t} \in \mathbb{C}^{M^2 \times M^2}$ represent predicted and target output value with regards to weight, w, respectively, \sum represents summation over all matrix elements, ϕ represents the argument function for a complex number input. We add an ℓ_2 regularization term to encourage generalization of the model with regularization parameter, $\alpha = 10^{-4}$. This formula implicitly weights the phase contributions by the product of magnitudes of the respective elements in $\widehat{\mathbf{A}_t}(w)$ and $\mathbf{A_t}$, which upon convergence will approximately equal the squared magnitude of the target.

The rationale for this is that when the optimization algorithm approaches a minimum, the remaining error for each complex element will be entirely due to aleatoric uncertainty, e.g. a circularly symmetric zero-mean complex Gaussian distribution³³. To estimate the correction factor, the element-wise complex errors can be summed, as shown in Supplementary Fig. 3c. This will produce an overall complex factor that has the desired global phase shift, shown in Supplementary Fig. 3d. The predicted output value can be corrected by multiplying by this phase factor as shown in Supplementary Fig. 3e, the result of which is then used to compute further parameter updates in the gradient descent algorithm. It can be seen that the complex error in Supplementary Fig. 3f between the predicted and target output value is reduced to a minimum after removing the phase factor

compared to that calculated by MAE. We then compared the absolute values of the complex error calculated by MAE (green bar) and our customized global phase insensitive loss function (blue bar) respectively over 100,000 pairs of predicted and desired TM as shown in Supplementary Fig. 3g. The error using the custom loss function is more than two times smaller than that of the conventional loss function (MAE).

Experimental measurement and updated model setup. The optical layout of our experimental setup is provided in ref. 12. Measuring the TM, treated as a linear operator, involves input modulation and output recovery. To achieve input modulation, the incident light was collimated into MMF by an objective lens and a 4f configuration after reflecting from digital micro-mirror device (DMD). In our specific case, the input fields are implemented using the Hadamard basis, providing an orthogonal set of modulated inputs. For the complex output recovery, images of the output facet of the fiber are captured using a movable calibration module. The light from the multimode fiber (MMF) is combined with the reference signal using a beam splitter. The reference light is directed to the camera through a single-mode fiber, and then the off-axis holography is recorded by CCD camera after magnifying by a microscope objective. By employing this optical layout, we are able to accurately measure the TM and gain insights into the propagation characteristics of light through the MMF. Using this approach, we measured experimental TMs for 164 different bending conformations and selected 64 rows and 64 columns of the raw measurements to create suitably sized matrices for training our model. TMs are measured at a wavelength of 488 nm and we use these as our base A_{λ_1} at wavelength λ_1 . We then scale this matrix to λ_{2-3} using the method in Eqs. (3)-(4), which has been validated previously on multi-wavelength TM datasets¹⁴.

For a small size matrix (8×8) we find that the model trained on simulation data is sufficient to reconstruct cropped 8 × 8 experimental matrices. However, for the larger 64 × 64 matrices, the model pre-trained on simulated data is prone to overfitting as it tends to also learn the prior distribution of TMs, and the subsequent loss is around 9.24% (standard deviation 0.78%). This learning of a prior can be advantageous in some cases where prior information is essential to resolve degeneracies, but to avoid that here we next re-trained the model with an augmented dataset containing 600,000 additional random matrices with elements drawn from complex uniform distribution. This reduced loss to an average value of around 5.07% (standard deviation of 0.67%), but a degree of overfitting is still present and so tweaked the model by continuing the training on 100 experimental TM, keeping 64 aside for validation and testing. Visually, these experimental TMs are structured differently to our simulated TM due to their use of a different basis. However, the training on random matrices seems to encourage generalization to different matrix structures.

Data availability

The data presented in this study are available from the following source: https://doi.org/10.17639/nott.7334.

Code availability

The code for this study is available from the following source: https://doi.org/10.17639/

Received: 30 March 2023; Accepted: 3 October 2023; Published online: 18 October 2023

References

- UK, C. R. Boston Scientific, Portfolio-group. https://www.bostonscientific.com/ content/dam/bostonscientific/endo/portfolio-group/spyglass/spyglass_detail_ brochure.pdf.
- Lee, C. M., Engelbrecht, C. J., Soper, T. D., Helmchen, F. & Seibel, E. J. Scanning fiber endoscopy with highly flexible, 1 mm catheterscopes for widefield, full-color imaging. *J. Biophoton.* 3, 385–407 (2010).
- Untracht, G. R., Karnowski, K. & Sampson, D. D. Imaging the small with the small: prospects for photonics in micro-endomicroscopy for minimally invasive cellular-resolution bioimaging. APL Photon. 6, 060901 (2021).
- Hwang, K. et al. Handheld endomicroscope using a fiber-optic harmonograph enables real-time and in vivo confocal imaging of living cell morphology and capillary perfusion. *Microsyst. Nanoeng.* 6, 72 (2020).
- Turtaev, S. et al. High-fidelity multimode fibre-based endoscopy for deep brain in vivo imaging. *Light Sci. Appl.* 7, 1–8 (2018).
- Psaltis, D. & Moser, C. Imaging with multimode fibers. Opt. Photon. News 27, 24 (2016).
- Gu, R. Y., Mahalati, R. N. & Kahn, J. M. Design of flexible multi-mode fiber endoscope. Opt. Express 23, 26905 (2015).
- Li, S., Horsley, S. A., Tyc, T., Čižmár, T. & Phillips, D. B. Memory effect assisted imaging through multimode optical fibres. *Nat. Commun.* 12, 3751 (2021).
- Li, A. et al. Focus scanning with feedback-control for fiber-optic nonlinear endomicroscopy. Biomed. Opt. Express 8, 2519–2527 (2017).
- Weiss, U. & Katz, O. Two-photon lensless micro-endoscopy with in-situ wavefront correction. Opt. Express 26, 28808–28817 (2018).
- Farahi, S., Ziegler, D., Papadopoulos, I. N., Psaltis, D. & Moser, C. Dynamic bending compensation while focusing through a multimode fiber. *Opt. Express* 21, 22504–22514 (2013).
- Wen, Z. et al. Single multimode fibre for in vivo light-field-encoded endoscopic imaging. Nat. Photon. 17, 679–687 (2023).
- Chen, H., Fontaine, N. K., Ryf, R., Neilson, D. T. & Winzer, P. Remote spatiotemporal focusing over multimode fiber enabled by single-ended channel estimation. *IEEE J. Sel. Top. Quant. Electron.* 26, 1–9 (2020).
- Gordon, G. S. et al. Characterizing optical fiber transmission matrices using metasurface reflector stacks for lensless imaging without distal access. *Phys. Rev. X* 9, 041050 (2019).
- Lee, S.-Y., Parot, V. J., Bouma, B. E. & Villiger, M. Efficient dispersion modeling in optical multimode fiber. *Light Sci. Appl.* 12, 31 (2023).
- Li, S. et al. Compressively sampling the optical transmission matrix of a multimode fibre. Light Sci. Appl. 10, 88 (2021).
- Huang, G., Wu, D., Luo, J., Huang, Y. & Shen, Y. Retrieving the optical transmission matrix of a multimode fiber using the extended kalman filter. Opt. Express 28, 9487 (2020).
- Rahmani, B., Loterie, D., Konstantinou, G., Psaltis, D. & Moser, C. Multimode optical fiber transmission with a deep learning network. *Light Sci. Appl.* 7, 69 (2018).
- Liu, Y. et al. Single-shot wide-field imaging in reflection by using a single multimode fiber. Appl. Phys. Lett. 122, 063701 (2023).
- Fan, P. et al. Deep learning enabled scalable calibration of a dynamically deformed multimode fiber. Adv. Photon. Res. 3, 2100304 (2022).
- Mouthaan, R., Christopher, P. J., Gordon, G. S., Wilkinson, T. D. & Euser, T. G. Robust correction of interferometer phase drift in transmission matrix measurements. *Appl. Opt.* 61, 4315–4321 (2022).
- Gordon, G. S. et al. Full-field quantitative phase and polarisation-resolved imaging through an optical fibre bundle. Opt. Express 27, 23929–23947 (2019).
- Wirkert, S. J. et al. Physiological parameter estimation from multispectral images unleashed. In Medical Image Computing and Computer Assisted Intervention-MICCAI 2017: 20th International Conference, Quebec City, QC, Canada, September 11-13, 2017, Proceedings, Part III 20, 134–141 (Springer, 2017).
- Osman, A., Crowley, J. & Gordon, G. D. Training generative adversarial networks for optical property mapping using synthetic image data. *Biomed. Opt. Express* 13, 5171–5186 (2022).
- Shorten, C. & Khoshgoftaar, T. M. A survey on image data augmentation for deep learning. J. Big Data 6, 1–48 (2019).

- Gordon, G. S., Mouthaan, R., Wilkinson, T. D. & Bohndiek, S. E. Coherent imaging through multicore fibres with applications in endoscopy. *J. Lightwave Technol.* 37, 5733–5745 (2019).
- Carpenter, J., Eggleton, B. J. & Schröder, J. 110x110 optical mode transfer matrix inversion. Opt. Express 22, 96–101 (2014).
- Arnold, L. On wigner's semicircle law for the eigenvalues of random matrices.
 Wahrscheinlichkeitstheorie verwandte Geb. 19, 191–198 (1971).
- Hile, G. N. & Lounesto, P. Matrix representations of clifford algebras. *Linear Algebra Appl.* 128, 51–63 (1990).
- Loterie, D. et al. Digital confocal microscopy through a multimode fiber. Opt. Express 23, 23845 (2015).
- Plöschner, M., Tyc, T. & Čižmár, T. Seeing through chaos in multimode fibres. Nat. Photon. 9, 529–535 (2015).
- Zheng, Y. & Gordon, G. AI and Optical Data Sciences IV, vol. 12438, 288–293 (SPIE, 2023).
- Bhatt, D. Variational Aleatoric Uncertainty Calibration In Neural Regression (2021).

Acknowledgements

The authors acknowledge support from a UKRI Future Leaders Fellowship (MR/T041951/1) and an EPSRC Ph.D. studentship.

Author contributions

Y.Z.: idea conception, code implementation, result analysis, and manuscript writing. T.W.: code implementation for confocal imaging. W.Z. and Q.Y.: collection of experimental data and manuscript writing. G.S.D.G.: idea conception, project supervision, and manuscript writing.

Competing interests

The authors declare no competing interests.

Additional information

Supplementary information The online version contains supplementary material available at https://doi.org/10.1038/s42005-023-01410-x.

Correspondence and requests for materials should be addressed to George S. D. Gordon.

Peer review information *Communications Physics* thanks the anonymous reviewers for their contribution to the peer review of this work.

Reprints and permission information is available at http://www.nature.com/reprints

Publisher's note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.



Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing,

adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit https://creativecommons.org/licenses/by/4.0/.

© The Author(s) 2023