# Modeling electrocortical activity through improved local approximations of integral neural field equations

S Coombes<sup>1</sup> and N A Venkov<sup>1</sup> and L Shiau<sup>2</sup> and I Bojak<sup>3</sup> and D T J Liley<sup>4</sup> and C R Laing<sup>5</sup>

<sup>1</sup> School of Mathematical Sciences, University of Nottingham, NG7 2RD, UK.

<sup>2</sup> Department of Mathematics, University of Houston, Houston, TX 77058, USA.

<sup>3</sup> Department of Cognitive Neuroscience, Radboud University Nijmegen Medical Centre,

Postbus 9101, 6500 HB Nijmegen, The Netherlands.

<sup>4</sup> Brain Sciences Institute, Swinburne University of Technology, PO Box 218, Victoria 3122, Australia.

<sup>5</sup> Institute of Information and Mathematical Sciences, Massey University,

Private Bag 102-904, North Shore Mail Centre, Auckland, New Zealand.

(Dated: October 3, 2007)

Neural field models of firing rate activity typically take the form of integral equations with space-dependent axonal delays. Under natural assumptions on the synaptic connectivity we show how one can derive an equivalent partial differential equation (PDE) model that properly treats the axonal delay terms of the integral formulation. Our analysis avoids the so-called *long-wavelength* approximation that has previously been used to formulate PDE models for neural activity in two spatial dimensions. Direct numerical simulations of this PDE model show instabilities of the homogeneous steady state that are in full agreement with a Turing instability analysis of the original integral model. We discuss the benefits of such a local model and its usefulness in modeling electrocortical activity. In particular we are able to treat "patchy" connections, whereby a homogeneous and isotropic system is modulated in a spatially periodic fashion. In this case the emergence of a "lattice-directed" traveling wave predicted by a linear instability analysis is confirmed by the numerical simulation of an appropriate set of coupled PDEs.

#### PACS numbers: 87.10.+e

#### I. INTRODUCTION

In many regions of mammalian neocortex, synaptic connectivity patterns follow a laminar arrangement, with strong vertical coupling between layers. Consequently cortical activity is considered as occurring on a two dimensional plane, with the coupling between layers ensuring near instantaneous vertical propagation. Hence, it is highly desirable to obtain solutions to fully planar neural field models. The most popular Wilson-Cowan [1] or Amari [2] style neural field models are typically written in the language of integro-differential or purely integral equations (see [3–5] for recent reviews). In recent years there has been a growing interest in neural field models where the communication between different parts of the domain is delayed due to the finite conduction speed of action potentials [6–10]. The advent of this work can be traced back to that of Nunez [11]. However, the set of mathematical techniques for the analysis of non-local models with space-dependent delays is not yet as thoroughly developed as it is for local partial differential equation (PDE) models. As discussed in [12] a local PDE model would offer a number of advantages over its non-local counterpart, allowing the use of i) powerful techniques from nonlinear PDE theory, ii) standard numerical techniques for the solution of PDEs, and iii) a more numerically straightforward analysis of the effects of spatial inhomogeneities. To date progress in this area has been made by Jirsa and Haken [13] for neural field models in one spatial dimension with axonal delays, and by Laing and Troy [14] in two spatial dimensions

for models lacking axonal delays. In both cases integral transform techniques are exploited and a PDE description is obtained only when the integral models under consideration are defined by spatio-temporal kernels whose Fourier transform has a rational polynomial structure. It is the goal of this paper to address the physiologically important case of a model in two spatial dimensions with axonal delays and to obtain an equivalent PDE model. Previous work on this problem by Liley et al. [12] has shown that for synaptic connectivity functions that fall off exponentially with distance, there is an equivalent local model consisting of an infinite set of PDEs involving fractional derivative terms. Although not particularly useful in its own right this system can be approximated by a single hyperbolic PDE. This PDE has been shown to provide a so-called *long-wavelength* approximation to the underlying integral model, and equations of this type have been used in several EEG modeling studies (see for example [15–17]).

In section II we introduce the class of neural field population models that we study in this paper. Next in section III we derive the equivalent PDE model, and compare it to the model obtained using the long-wavelength approximation. In section IV we present a Turing instability analysis of the original integral model. Importantly we show that numerical simulations of the PDE model are in precise agreement with the behavior predicted at the onset of a Turing instability. The case of spatially modulated synaptic connectivity is treated in section V. Finally, in section VI we discuss natural extensions of the work in this paper.

#### II. INTEGRAL NEURAL FIELD MODEL

We consider planar neural field models that incorporate delayed synaptic interactions between distinct neuronal populations where the activity of synapses in population a induced by activity in population b can be written

$$u_{ab} = \eta_{ab} * \psi_{ab}. \tag{1}$$

Here  $u_{ab} = u_{ab}(\mathbf{r}, t)$ ,  $\mathbf{r} = (r, \theta)$   $(r \in \mathbb{R}^+, \theta \in [0, 2\pi), t \in \mathbb{R}^+)$ , and a and b label functionally homogeneous neuronal populations. The activity variable  $u_{ab}(\mathbf{r}, t)$  can be interpreted as a spatially averaged synaptic activity centered about  $\mathbf{r}$ . The symbol \* represents a temporal convolution in the sense that

$$(\eta * \psi)(\mathbf{r}, t) = \int_0^t \mathrm{d}s \eta(s) \psi(\mathbf{r}, t - s). \tag{2}$$

The variable  $\psi_{ab}(\mathbf{r},t)$  describes the presynaptic input to population a arriving from population b, which we write

$$\psi_{ab}(\mathbf{r},t) = \int_{\mathbb{R}^2} d\mathbf{r}' w_{ab}(\mathbf{r},\mathbf{r}') f_b \circ h_b(\mathbf{r}',t-|\mathbf{r}-\mathbf{r}'|/v_{ab}).$$
(3)

The function  $\eta_{ab}(t)$  (with  $\eta_{ab}(t) = 0$  for t < 0) represents a normalised synaptic filter, whilst  $w_{ab}(\mathbf{r}, \mathbf{r}')$ is a synaptic footprint describing the anatomy of network connections. One common choice for the synaptic filter is the so-called delayed difference of exponentials:  $\eta_{ab}(t) = \eta(t - \tau_{ab}; \alpha_{ab}, \beta_{ab})$ , where  $\eta(t; \alpha, \beta) = (1/\alpha - 1/\beta)^{-1} [e^{-\alpha t} - e^{-\beta t}] \Theta(t)$  and  $\tau_{ab}$  is a mean synaptic processing delay between populations a and b. Here,  $\Theta(t)$  is the Heaviside step function. In the absence of detailed anatomical data it is common practice to consider cortico-cortical connectivity functions to be homogeneous and isotropic so that  $w_{ab}(\mathbf{r}, \mathbf{r}') = w_{ab}(|\mathbf{r} - \mathbf{r}'|)$ . The function  $f_a$  represents the firing rate of population a, and  $v_{ab}$  is the mean synaptic axonal velocity along a fibre connecting population b to population a. For conduction velocities in the range 1.5–7 m/s (typical of white matter axons) axonal delays are significant over scales ranging from a single cortical area (of spatial scale 10mm) up to the scale of inter-hemispherical collosal connections.

In a Wilson-Cowan or Amari style neural field model the variables  $h_a$  are taken to be of the form  $h_a = \sum_b u_{ab} + h_a^0$ , with  $h_a^0$  a constant drive term. In more sophisticated models of EEG activity, such as in the work of Liley et al. [12],  $h_a$  is interpreted as the average soma membrane potential of a population and chosen to obey a nonlinear equation of the form

$$(1 + \tau_a \partial_t) h_a = \sum_b \Gamma_{ab}(h_a) u_{ab} + h_a^0.$$
 (4)

Here the activity dependent functions  $\Gamma_{ab}$  weight the contributions from the various contributing neuronal populations, and take into account the shunting nature of synaptic interactions (see [12] for details).

## III. EQUIVALENT PDE MODEL

The numerical solution of the neural field model defined in section II is challenging for two reasons in particular. The first being that the non-local presynaptic input term (3) is defined by an integral over a two-dimensional spatial domain, and the second that it involves an argument that is delayed in time. In fact since this delay term is space-dependent it requires keeping a memory of all previous synaptic activity. One of the key motivations of our work is to circumvent the huge numerical overheads in simulating such a delayed non-local system.

Introducing  $G_{ab}(\mathbf{r},t) = G_{ab}(r,t)$  (where  $r = |\mathbf{r}|$ ) with

$$G_{ab}(r,t) = w_{ab}(r)\delta(t - r/v_{ab}), \tag{5}$$

allows us to re-write (3) as

$$\psi_{ab}(\mathbf{r},t) = \int_{-\infty}^{\infty} ds \int_{\mathbb{R}^2} d\mathbf{r}' G_{ab}(|\mathbf{r} - \mathbf{r}'|, t - s) \rho_b(\mathbf{r}', s), (6)$$

where  $\rho_a = f_a \circ h_a$ . Importantly the right hand side of (6) has a convolution structure. Introducing the 3D Fourier transform according to

$$\psi(\mathbf{r},t) = \frac{1}{(2\pi)^3} \int_{\mathbb{R}^3} d\mathbf{k} d\omega \psi(\mathbf{k},\omega) e^{i(\mathbf{k}\cdot\mathbf{r}+\omega t)}, \qquad (7)$$

then we find that  $G_{ab}(\mathbf{k},\omega) = G_{ab}(k,\omega)$ ,  $(k=|\mathbf{k}|)$  where

$$G_{ab}(k,\omega) = 2\pi \int_0^\infty w_{ab}(r) J_0(kr) r e^{-i\omega r/v_{ab}} dr.$$
 (8)

Here  $J_0(z)=(2\pi)^{-1}\int_0^{2\pi}\mathrm{d}\theta\mathrm{e}^{iz\cos\theta}$  is the Bessel function of the first kind of order zero. We recognize (8) as the Hankel transform of  $w_{ab}(r)\mathrm{e}^{-i\omega r/v_{ab}}$ .

If  $G_{ab}(k,\omega)$  can be represented in the form  $R_{ab}(k^2,i\omega)/P_{ab}(k^2,i\omega)$  then we have that  $P_{ab}(k^2,i\omega)\psi_{ab}(k,\omega)=R_{ab}(k^2,i\omega)\rho_b(k,\omega)$ . By identifying  $k^2\leftrightarrow -\nabla^2$  and  $i\omega\leftrightarrow\partial_t$ , then a formal inverse Fourier transform will yield a local model in terms of the operators  $\nabla^2$  and  $\partial_t$ . However, unless the functions  $P_{ab}$  and  $R_{ab}$  are polynomial in their arguments then the interpretation of functions of these operators is unclear. To illustrate this we revisit the common choice:

$$w_{ab}(r) = w_{ab}^0 e^{-r/\sigma_{ab}}/(2\pi),$$
 (9)

for which

$$G_{ab}(k,\omega) = w_{ab}^0 \frac{A_{ab}(\omega)}{(A_{ab}^2(\omega) + k^2)^{3/2}},$$
 (10)

where  $A_{ab}(\omega) = \sigma_{ab}^{-1} + i\omega/v_{ab}$ . Introducing the operator  $A_{ab}$ :

$$\mathcal{A}_{ab} = \left(\frac{1}{\sigma_{ab}} + \frac{1}{v_{ab}}\partial_t\right)^2,\tag{11}$$

then the problem arises as how to interpret  $[A_{ab} - \nabla^2]^{3/2}$ . In the long-wavelength approximation one merely expands  $G_{ab}(k,\omega)$  around k=0 for small k, yielding a

"nice" rational polynomial structure which is then manipulated as described above to give the PDE:

$$\left(\mathcal{A}_{ab} - \frac{3}{2}\nabla^2\right)\psi_{ab} = w_{ab}^0\rho_b. \tag{12}$$

We refer to (12) as the long-wavelength model. Higher order approximations can be obtained by expanding to higher powers in k [18], although all resulting higher order PDE models will still be long-wavelength approximations

To obtain a PDE model that side-steps the need to make the long-wavelength approximation we use the observation that  $e^{-r}$  can be fitted with a two-parameter function of the form [19]

$$E(r) = (\epsilon_1^2 - \epsilon_2^2)^{-1} \left[ K_0(r/\epsilon_1) - K_0(r/\epsilon_2) \right],$$
 (13)

where  $K_0$  is the modified Bessel function of the second kind of order zero. The prefactor  $(\epsilon_1^2 - \epsilon_2^2)^{-1}$  ensures a common normalisation for  $e^{-r}$  and E(r).

The form of equation (13) motivates the approximation  $e^{-r/\sigma}e^{-i\omega r/v} \approx (\epsilon_1^2 - \epsilon_2^2)^{-1}[K_0(A_{ab;\epsilon_1}(\omega)r) - K_0(A_{ab;\epsilon_2}(\omega)r)]$ , where  $A_{ab;\epsilon}(\omega)$  is obtained under the replacement of  $\sigma$  by  $\epsilon\sigma$  in  $A_{ab}(\omega)$ . This form is particularly useful since  $K_0(ar)$  has a simple Hankel transform given by  $1/(a^2 + k^2)$ . For this choice  $G_{ab}(k,\omega)$  takes the form

$$\frac{w_{ab}^{0}}{\epsilon_{1}^{2} - \epsilon_{2}^{2}} \left[ \frac{1}{(A_{ab;\epsilon_{1}}^{2}(\omega) + k^{2})} - \frac{1}{(A_{ab;\epsilon_{2}}^{2}(\omega) + k^{2})} \right]. \quad (14)$$

In this case we obtain the PDE model:

$$(\mathcal{A}_{ab;\epsilon_1} - \nabla^2)(\mathcal{A}_{ab;\epsilon_2} - \nabla^2)\psi_{ab} = w_{ab}^0 \mathcal{B}_{ab}\rho_b, \qquad (15)$$

where

$$\mathcal{B}_{ab} = \frac{1}{\epsilon_1^2 \epsilon_2^2 \sigma_{ab}^2} \left[ 1 + \frac{2\epsilon_1 \epsilon_2 \sigma_{ab}}{v_{ab} (\epsilon_1 + \epsilon_2)} \partial_t \right]. \tag{16}$$

For want of a better name we shall refer to (15) as the rational model. Note that the long-wavelength model can also be obtained using the approximation  $e^{-r} \approx L(r) = 2K_0(\sqrt{2/3}r)/3$ . However, this approximation is poor for both small and large values of r since  $\lim_{r\to 0,\infty} L(r)/e^{-r} = \infty$ . Note that  $\lim_{r\to 0} E(r) = (\epsilon_1^2 - \epsilon_2^2)^{-1} \ln(\epsilon_1/\epsilon_2)$ , and so is well behaved at the origin. A plot of E(r) (rational model) and L(r) (long-wavelength model) is shown in Fig. 1. The long-wavelength model is recovered from the rational model with the choice  $(\epsilon_1, \epsilon_2) = (\sqrt{3/2}, 0)$ .

We note that the formulation of the rational model (and indeed the long-wavelength model) provides only an approximation to the original relationship  $G_{ab}(r,t) = w_{ab}(r)\delta(t-r/v_{ab})$ . As a result synaptic activity does not just arrive at  $t = r/v_{ab}$ . This is best seen by deriving  $G_{ab}(r,t)$  for the choice (14). Writing the inverse transform of  $1/(A_{ab}^2(\omega) + k^2)$  as  $H_{ab}(r,t)$  (calculated in Appendix A) we have that  $G_{ab}(r,t) = (\epsilon_1^2 - \epsilon_1^2)$ 

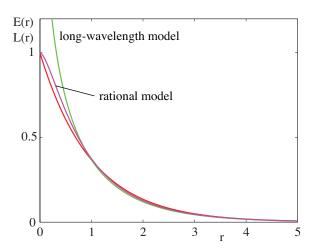


FIG. 1: (Color online). A plot of E(r) (rational model) with  $(\epsilon_1, \epsilon_2) = (\sqrt{3/2}, \epsilon)$ , and L(r) (long-wavelength model) is shown together with a plot of  $e^{-r}$ . In this illustrative plot we have chosen  $\epsilon$  as the root of  $\epsilon_1^2 - \epsilon^2 - \ln(\epsilon_1/\epsilon)$ , so as to fix E(0) = 1.

$$(\epsilon_2^2)^{-1} w_{ab}^0 [H_{ab;\epsilon_1}(r,t) - H_{ab;\epsilon_2}(r,t)],$$
 which gives

$$G_{ab}(r,t) = w_{ab}^{0} \frac{v_{ab}\Theta(v_{ab}t - r)}{2\pi\sqrt{v_{ab}^{2}t^{2} - r^{2}}} \times \left(\epsilon_{1}^{2} - \epsilon_{2}^{2}\right)^{-1} \left[ e^{-v_{ab}t/(\epsilon_{1}\sigma_{ab})} - e^{-v_{ab}t/(\epsilon_{2}\sigma_{ab})} \right].$$
(17)

Although the shape of G(r,t) is consistent with our physical expectations, namely a positive decaying pulse beyond  $t = r/v_{ab}$ , we have as yet not fixed the parameters  $(\epsilon_1, \epsilon_2)$  of the rational model. To do this we could try and approximate the complex function (10) of the full model using (14). However, a simpler approach is to consider fitting a projection of (10) that describes the linear stability of the homogeneous steady state. We do this in the next section. Here we show that the dynamic pattern forming instability borders for the rational model are in closer quantitative agreement to those of the full model than the long-wavelength model. In this sense we argue that the rational model is an improvement over the long-wavelength model (which it recovers as a special case).

We can also interpret the above in terms of a distance dependent distribution of velocities  $q_{ab}(v, r)$  for the spreading of synaptic activity by writing

$$G_{ab}(r,t) = w_{ab}(r) \int_0^\infty dv \, q_{ab}(v,r) \delta(t-r/v)$$
$$= w_{ab}(r) \frac{v^2}{r} q_{ab}(v,r) \Big|_{v=r/t} , \qquad (18)$$

with the normalization  $\int_0^\infty \mathrm{d}v\, q_{ab}(v,r)=1$ . The original definition (8) is recovered for a single conduction velocity  $q_{ab}(v,r)=\delta(v-v_{ab})$ . Rearranging (18) gives the velocity

distribution as

$$q_{ab}(v,r) = \frac{r}{v^2} \frac{G_{ab}(r,r/v)}{w_{ab}(r)}.$$
 (19)

Using (17) we find that, for both the rational and long-wavelength model, the distribution  $q_{ab}(v,r)$  has a peak at  $v=v_{ab}$  as expected, as well as one for small r and v. This second peak however is strongly localized and hence merely introduces an insignificant overall delay to a traveling pulse.

#### IV. TURING INSTABILITY ANALYSIS

Here we explore the stability of the homogeneous steady state for the choice  $h_a = \sum_b u_{ab} + h_a^0$ . The extension of this analysis to include the Liley model given by (4) is straightforward. Let  $h_a(\mathbf{r},t) = h_a^{\rm ss}$  denote the homogeneous steady state, defined by  $h_a^{\rm ss} = \sum_b W_{ab} f_b(h_b^{\rm ss}) + h_a^0$ , where  $W_{ab} = \int_{\mathbb{R}^2} \mathrm{d}\mathbf{r}' w_{ab}(\mathbf{r}')$ . Linearizing around this solution and considering perturbations of the form  $h_a(\mathbf{r},t) = \overline{h}_a \mathrm{e}^{\lambda t} \mathrm{e}^{i\mathbf{k}\cdot\mathbf{r}}$ , gives the system of equations

$$\overline{h}_a = \sum_b \widetilde{\eta}_{ab}(\lambda) G_{ab}(k, -i\lambda) \gamma_b \overline{h}_b.$$
 (20)

Here  $\widetilde{\eta}_{ab}(\lambda) = \int_0^\infty \mathrm{d}s \mathrm{e}^{-\lambda s} \eta_{ab}(s)$  is the Laplace transform of  $\eta_{ab}(t)$  and  $\gamma_a = f_a'(h_a^{\mathrm{ss}})$ . Demanding non-trivial solutions yields an equation for the continuous spectrum  $\lambda = \lambda(k)$  in the form  $\mathcal{E}(k,\lambda) = 0$ , where  $\mathcal{E}(k,\lambda) = \det(\mathcal{D}(k,\lambda) - I)$ , and

$$[\mathcal{D}(k,\lambda)]_{ab} = \widetilde{\eta}_{ab}(\lambda)G_{ab}(k,-i\lambda)\gamma_b. \tag{21}$$

Note that for a delayed difference of exponentials function we have simply that

$$\widetilde{\eta}_{ab}(\lambda) = \frac{e^{-\lambda \tau_{ab}}}{(1 + \lambda/\alpha_{ab})(1 + \lambda/\beta_{ab})}.$$
(22)

An instability occurs when for the first time there are values of k at which the real part of  $\lambda$  is nonnegative. A Turing bifurcation point is defined as the smallest value of some order parameter for which there exists some nonzero  $\mathbf{k}_c$  satisfying Re  $(\lambda(k_c)) = 0$ . It is said to be static if Im  $(\lambda(k_c)) = 0$  and dynamic if Im  $(\lambda(k_c)) \equiv \omega_c \neq 0$ . The dynamic instability is often referred to as a Turing-Hopf bifurcation and generates a global pattern with wavenumber  $k_c$ , which moves coherently with a speed  $c = \omega_c/k_c$ , i.e. as a periodic traveling wave train. Generically one expects to see the emergence of doubly periodic solutions that tessellate the plane, namely traveling waves with hexagonal, square or rhombic structure. If the maximum of the dispersion curve is at k=0 then the mode that is first excited is another spatially uniform state. If  $\omega_c \neq 0$ , we expect the emergence of a homogeneous limit cycle with temporal frequency  $\omega_c$ .

For computational purposes it is convenient to split the dispersion relation into real and imaginary parts and write  $\lambda = \nu + i\omega$  to obtain

$$\mathcal{E}_R(\nu,\omega) = 0, \qquad \mathcal{E}_I(\nu,\omega) = 0,$$
 (23)

where  $\mathcal{E}_R(\nu,\omega) = \text{Re } \mathcal{E}(k,\nu+i\omega)$  and  $\mathcal{E}_I(\nu,\omega) = \text{Im } \mathcal{E}(k,\nu+i\omega)$ . Solving the system of equations (23) gives us a curve in the plane  $(\nu,\omega)$  parameterized by k. A static bifurcation may thus be identified with the tangential intersection of  $\omega = \omega(\nu)$  along the line  $\nu = 0$  at the point  $\omega = 0$ . Similarly a dynamic bifurcation is identified with a tangential intersection at  $\omega \neq 0$ . This is equivalent to tracking points where  $\nu'(\omega) = 0$ , given by the equation  $\partial_k \mathcal{E}_R \partial_\omega \mathcal{E}_I - \partial_k \mathcal{E}_I \partial_\omega \mathcal{E}_R = 0$ .

For example, consider two populations, one excitatory and one inhibitory, and use the labels  $a \in \{E, I\}$ , with  $w^0_{EE,IE} > 0$  and  $w^0_{II,EI} < 0$ . In this case

$$\mathcal{E}(k,\lambda) = [1 - \widetilde{\eta}_{II}G_{II}\gamma_I][1 - \widetilde{\eta}_{EE}G_{EE}\gamma_E] - \widetilde{\eta}_{EI}\widetilde{\eta}_{IE}G_{EI}G_{IE}\gamma_I\gamma_E,$$
 (24)

where  $G_{ab} = G_{ab}(k, -i\lambda)$  and  $\widetilde{\eta}_{ab} = \widetilde{\eta}_{ab}(\lambda)$ . For simplicity we shall set  $\alpha_{aI} = \beta_{aI} = 1$  and  $\alpha_{aE} = \beta_{aE} = \alpha$ and ignore synaptic delays by taking  $\tau_{ab} = 0$ . In neocortex the extent of excitatory connections  $W_{aE}$  is broader than that of inhibitory connections  $W_{aI}$ , and so we take  $\sigma_{aE} > \sigma_{aI}$ . Again for simplicity we set  $\sigma_{aI} = \sigma_{I} = 1$  and  $\sigma_{aE} = \sigma_E$ . For a common choice of firing rate function  $f_a = f$  we may also set  $\gamma_a = \gamma$ . Finally we focus on only a single axonal conduction velocity and set  $v_{ab} = v$ . In Fig. 2 we show a plot of the critical curves in the  $(v,\gamma)$  plane above which the homogeneous steady state is unstable to dynamic instabilities with  $k_c = 0$  (bulk oscillations) and  $k_c \neq 0$  (traveling waves). The upper panel in Fig. 2 shows results for the full model (defined by (9)), the middle panel that for the long-wavelength model, and the lower is that for the rational model. We note that there are no qualitative differences between the models in the sense that, at the linear level, all models support Hopf and Turing-Hopf instabilities, with a switch from one to the other with increasing v. One obvious difference is that with an appropriate choice of  $(\epsilon_1, \epsilon_2)$  the rational model is in far better quantitative agreement with the full model. To test the predictions of our linear stability analysis and to compare the nonlinear behaviour of the two models we resort to direct numerical simulations. Necessarily this requires the choice of a firing rate function.

In all direct numerical simulations of the PDE models we take the sigmoidal form

$$f(h) = \frac{1}{1 + e^{-\beta h}}. (25)$$

Here  $\beta$  is a gain parameter. Without loss of generality we set the steady state value of  $h_{E,I}$  to be zero, giving  $\gamma = f'(0) = \beta/4$ . The predictions of the linear stability analysis are found to be in excellent agreement with the

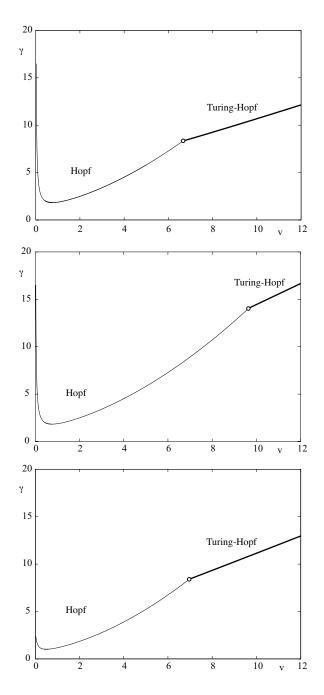


FIG. 2: Critical curves showing the instability thresholds for dynamic instabilities in the  $(v,\gamma)$  plane. Top: Full model. Middle: Long-wavelength model. Bottom: Rational model with  $(\epsilon_1,\epsilon_2)=(0.6,0.6)$ . Parameters  $\alpha=1,\,w_{EE}^0=w_{IE}^0=1,\,w_{II}^0=w_{EI}^0=-4,\,h_E^0=h_I^0=0$  and  $\sigma_E=2$ .

behavior of the PDE models. Figure 3 shows a pattern seen in the long-wavelength model, beyond the Turing-Hopf bifurcation, while Figure 4 shows a pattern seen in the rational model, also beyond the Turing-Hopf bifurcation. For both models parallel moving stripes are very commonly seen beyond the Turing-Hopf bifurcation, particularly for small domains, but a variety of other pat-

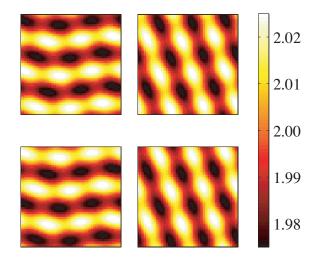


FIG. 3: (Color online). Left to right, top to bottom: snapshots of a periodic pattern for the long-wavelength model, each 1/4 of a period later than the previous one.  $u_{EE}$  is shown. Domain is  $30 \times 30$ .  $v = 12, \gamma = 20$ . Other parameters are as in Fig. 2.

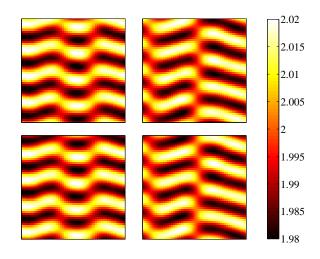


FIG. 4: (Color online). Left to right, top to bottom: snapshots of a periodic pattern for the rational model, each 1/4 of a period later than the previous one.  $u_{EE}$  is shown. Domain is  $30 \times 30$ . v = 12,  $\gamma = 15$ . Other parameters are as in Fig. 2.

terns such as those shown here are also possible, i.e. both systems have multiple attractors. Therefore, based upon numerics alone it is not possible to make the statement that there is a qualitative difference between the types of possible patterns in the two models. A short discussion of the numerical techniques used in this paper can be found in Appendix B.

### V. SPATIAL MODULATION

It is now known that the neocortex has a crystalline micro-structure at the millimeter length scale, so that the assumption of isotropic connectivity has to be revised (for a recent discussion see [20]). For example, in visual cortex it has been shown that long range horizontal connections (extending several millimeters) tend to link neurons having common functional properties (as defined by their feature maps). Since the feature maps (for orientation preference, spatial frequency preference and ocular dominance) are approximately periodic this leads to patchy connections that break continuous rotation symmetry (but not necessarily continuous translation symmetry). With this in mind we introduce a periodically modulated spatial kernel of the form

$$w_{ab}^{\mathrm{P}}(\mathbf{r}, \mathbf{r}') = w_{ab}(|\mathbf{r} - \mathbf{r}'|) J_{ab}(\mathbf{r} - \mathbf{r}'), \tag{26}$$

where  $J_{ab}(\mathbf{r})$  varies periodically with respect to a regular planar lattice  $\mathcal{L}$ . Note that the patchy kernel  $w_{ab}^P$  is homogeneous, but not isotropic. Following recent work of Robinson [21] on *patchy propagators* we show how to obtain an equivalent PDE model for an integral neural field equation with a spatial kernel given by (26).

First we exploit the periodicity of  $J_{ab}(\mathbf{r})$  and represent it with a Fourier series:

$$J_{ab}(\mathbf{r}) = \sum_{\mathbf{q}} J_{ab}^{\mathbf{q}} e^{i\mathbf{q} \cdot \mathbf{r}}.$$
 (27)

The vectors  $\mathbf{q}$  are the reciprocal lattice vectors of the underlying lattice  $\mathcal{L}$ , and  $J_{ab}^{\mathbf{q}}$  are Fourier coefficients given by  $(2\pi)^{-2}\int_{\mathbb{R}^2}\mathrm{d}\mathbf{r}\mathrm{e}^{-i\mathbf{q}\cdot\mathbf{r}}J_{ab}(\mathbf{r})$ , with  $J_{ab}^{-\mathbf{q}}=(J_{ab}^{\mathbf{q}})^{\dagger}$  (where  $\dagger$  denotes complex-conjugation). In this case  $\psi_{ab}(\mathbf{k},\omega)=G_{ab}^{\mathbf{p}}(\mathbf{k},\omega)\rho_b(\mathbf{k},\omega)$ , where

$$G_{ab}^{P}(\mathbf{k},\omega) = \sum_{\mathbf{q}} J_{ab}^{\mathbf{q}} G_{ab}(|\mathbf{k} - \mathbf{q}|, \omega),$$
 (28)

and  $G_{ab}(\mathbf{k},\omega)$  is given by (8). We may then write  $\psi_{ab}(\mathbf{r},t) = \sum_{\mathbf{q}} J_{ab}^{\mathbf{q}} \psi_{ab}^{\mathbf{q}}(\mathbf{r},t)$ , where  $\psi_{ab}^{\mathbf{q}}(\mathbf{k},\omega) = G_{ab}(|\mathbf{k} - \mathbf{q}|,\omega)\rho_b(\mathbf{k},\omega)$ . Choosing  $G_{ab}(k,\omega)$  according to (14) we see that  $\psi_{ab}^{\mathbf{q}}(\mathbf{r},t)$  satisfies

$$(\mathcal{A}_{ab;\epsilon_1} - \nabla_{\mathbf{q}}^2)(\mathcal{A}_{ab;\epsilon_2} - \nabla_{\mathbf{q}}^2)\psi_{ab}^{\mathbf{q}} = w_{ab}^0 \mathcal{B}_{ab}\rho_b, \qquad (29)$$

where  $\nabla_{\mathbf{q}} = (\nabla - i\mathbf{q})$ . Hence, we have an infinite set of PDEs for the complex amplitudes  $\psi_{ab}^{\mathbf{q}}$  indexed by the reciprocal lattice vectors  $\mathbf{q}$ . Since  $\psi_{ab}^{-\mathbf{q}} = (\psi_{ab}^{\mathbf{q}})^{\dagger}$  then  $\psi_{ab}(\mathbf{r},t) = \sum_{\mathbf{q}} J_{ab}^{\mathbf{q}} \psi_{ab}^{\mathbf{q}}(\mathbf{r},t) \in \mathbb{R}$  as required. Assuming that there is a natural cut-off in  $\mathbf{q}$ , then we need only evolve a finite subset of these PDEs to see the effects of patchy connections on solution behavior. Note also that the Turing instability analysis for the patchy model is identical to that of the isotropic model under the replacement of  $G_{ab}$  by (28) in (21), so that now  $\lambda$  depends on the direction as well as the magnitude of  $\mathbf{k}$ . For the mode selected by the Turing mechanism all other modes

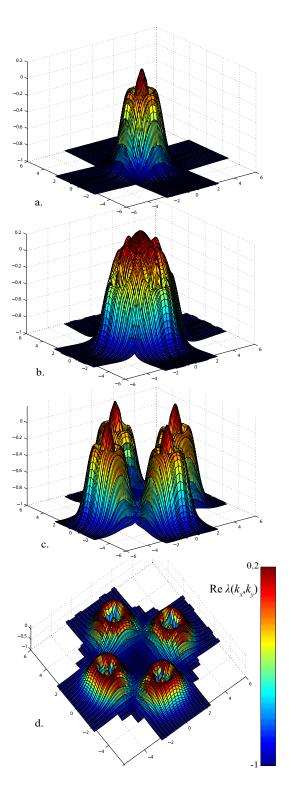


FIG. 5: (Color online). The dispersion surfaces Re  $\lambda(\mathbf{k})$  for fixed parameters: a.  $d=\infty$  (unmodulated model),  $v=4,\gamma=5$ ; b.  $d=4,v=4,\gamma=15$ ; c.  $v=4,d=2,\gamma=20$ ; d.  $v=10,d=4,\gamma=50$ . The values of  $\gamma$  are chosen so that the homogeneous steady state is just unstable. The peaks in the surfaces are *pinned* by the lattice wavevectors  $\pm \mathbf{k}_{1,2}, |\mathbf{k}_{1,2}| = 2\pi/d$ .

generated by discrete rotations of the reciprocal lattice will also be selected. Thus periodic patchy connections favour the generation of periodic patterns.

For example, consider a square lattice with length-scale d. The generators of the reciprocal lattice are  $\mathbf{k}_1 = 2\pi/d(1,0)$  and  $\mathbf{k}_2 = 2\pi/d(0,1)$ . Now choose  $J_{ab}(\mathbf{r}) = [\cos(\mathbf{k}_1 \cdot \mathbf{r}) + \cos(\mathbf{k}_2 \cdot \mathbf{r})]/2$ . In this case  $J_{ab}^{\mathbf{q}} = [\delta(\mathbf{q} - \mathbf{k}_1) + \delta(\mathbf{q} + \mathbf{k}_1) + \delta(\mathbf{q} - \mathbf{k}_2) + \delta(\mathbf{q} + \mathbf{k}_2)]/4$ , and we need only consider two coupled complex PDEs (indexed by  $\mathbf{k}_{1,2}$ ).

In Fig. 5 we plot the dispersion surfaces Re  $\lambda(\mathbf{k})$ ,  $\mathbf{k} = (k_x, k_y)$ , for parameters selected just beyond the instability of the homogeneous steady state. In the limit  $d \to \infty$  we recover the unmodulated model. For finite d we find that each lattice wavevector  $\pm \mathbf{k}_{1,2}$  introduces a shifted copy of the peak of the dispersion surface from the unmodulated case (Fig. 5a). When these peaks are widely separated (for lattice spacing  $d \leq 3$ ) the interaction between them is weak and the bifurcation parameter portrait is expected to be analogous to that of the unmodulated model (Fig. 2) (at least up to a factor of 4 coming from the particular choice of  $J_{ab}^{\mathbf{q}}$  above). In Fig. 6 we plot the bifurcations for the modulated model. Compared to the unmodulated case the Hopf bifurcation is transformed to a Turing-Hopf bifurcation with critical wavevectors coinciding with those of the lattice and independent of the axonal velocity v. This is associated with the central peaks at  $\pm \mathbf{k}_{1,2}$  in Fig. 5c crossing through zero from below. With increasing v the dominant bifurcation is also of Turing-Hopf type. However, in this case it is a ring of wavevectors surrounding  $\pm \mathbf{k}_{1,2}$  that go unstable first, as in Fig. 5d. In both cases this suggests the emergence of traveling waves aligned to the lattice size and direction, which are indeed observed in direct numerical simulations. We shall refer to these as "lattice-directed" traveling waves. In the regime  $3 \lesssim d \lesssim 6$  four wavevectors become unstable with  $|k_x| = |k_y|$ , as in Fig. 5b , and for  $d \gtrsim 6$  the system is effectively that of the unmodulated case described by Fig. 5a.

In Fig. 7 we plot the speed of a traveling wave at the Turing-Hopf bifurcation at v=1. The speed of the wave is seen to increase almost linearly with the spacing of the square lattice, d. This reflects the fact that for small d, the emergent frequency  $\omega_c$  is independent of d and  $k_c$  coincides with  $|\mathbf{k}_{1,2}|$ . The linear analysis predicting emergent wave speed is found to be in excellent agreement with direct numerical simulations. Figure 8 shows a lattice-directed traveling wave created in the Turing-Hopf bifurcation shown in Fig. 6, for v=1.

In Fig. 9 we show a pattern generated in the Turing-Hopf bifurcation for the system with a periodically-modulated kernel for v=10. It emerged from the spatially uniform state at the value of  $\gamma$  predicted from Fig. 6. The pattern is compatible with the wavenumber k for which the spatially uniform state is unstable.

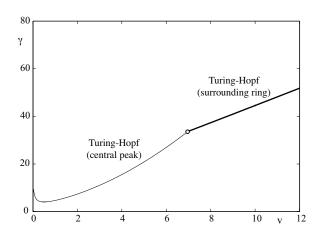


FIG. 6: Critical curves showing the Turing-Hopf instabilities in the  $(v,\gamma)$  plane for the rational model (15), with a periodically modulated kernel. In this example the underlying lattice is square, with spacing d. Parameters are as in Fig. 2 with d=1.

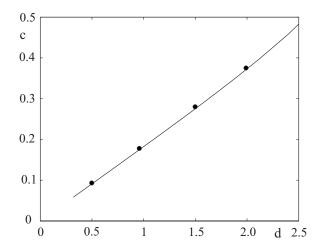


FIG. 7: Speed  $(c = \omega_c/k_c)$  of a lattice-directed traveling wave at the Turing-Hopf bifurcation shown in Fig. 6 for v=1 as a function of square lattice spacing d. The speed of the wave is seen to increase almost linearly with d. Here v=1 and other parameters are as in Fig. 2. The circles denote the results from direct numerical simulations.

# VI. CONCLUSIONS

Neural field models of firing rate activity have had a major impact in helping to develop an understanding of the dynamics of EEG [12, 22, 23]. In this paper we have shown how to write down an equivalent PDE model for a neural field model in two spatial dimensions with a particular form of decaying connectivity and a space-dependent axonal delay. Importantly this has avoided the so-called *long-wavelength* approximation that has been used in many EEG models to date. Direct numerical simulations of the equivalent PDE model

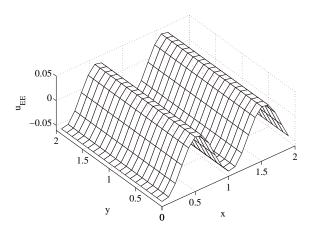


FIG. 8: Turing-Hopf pattern for patchy propagation.  $u_{EE}$  is shown at one instant in time.  $v=1, \gamma=10, d=1$ . The speed is  $\sim 0.182$  in the x direction. Other parameters are as in Fig. 2.

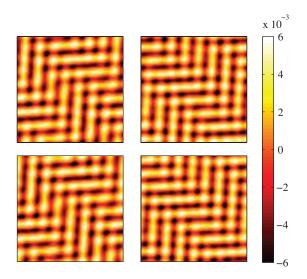


FIG. 9: (Color online). Left to right, top to bottom: snapshots of a periodic pattern for the rational model with patchy connections, each 1/4 of a period later than the previous one.  $u_{EE}$  is shown. The domain is  $7 \times 7$ , v = 10,  $\gamma = 50$ , d = 1 and other parameters as in Fig. 2.

have been shown to be consistent with a linear instability analysis of the original integral neural field model. Moreover, we have extended our approach to allow for patchy connections and used simulations of an appropriate set of coupled PDEs to confirm the existence of lattice-directed traveling waves.

A number of natural extensions of the work presented here are possible. The first concerns pattern selection; linear stability analysis alone cannot distinguish which of the doubly periodic solutions (hexagon, square, rhombus) will be excited first. To do this requires a further

weakly nonlinear analysis. Techniques to do this for integral models in one spatial dimension with axonal delays have recently been developed in [24], and are naturally generalized to two spatial dimensions. To further cope with patchy connections one may well be able to borrow from techniques developed for the study of amplitude equations in anisotropic PDE models [25]. Another extension would be to use the ideas presented here to discover if axonal delays have any significant effect on the existence and stability of other patterns seen in twodimensional neural fields such as spiral waves [26] and spatially-localised bumps [14, 27]. The treatment of distributed transmission speeds [28–30] is another important area, as is the extension to heterogeneous connection topologies (more realistic of real cortical structures) [20, 31] and addressing parameter heterogeneity (describing more realistic physiological scenarios) [17]. All of these are topics of ongoing activity and will be reported upon elsewhere.

## Acknowledgments

SC would like to acknowledge support from the EPSRC through the award of an Advanced Research Fellowship, Grant No. GR/R76219. The work of LS was supported in part by NSF Grant DMS-0244529. IB is supported by grant DP0209218 from the Australian Research Council.

## Appendix A

We calculate  $H_{ab}(r,t)$  as an inverse Fourier transform [32], namely

$$H_{ab}(r,t) = \frac{1}{(2\pi)^3} \int_{\mathbb{R}^3} d\mathbf{k} d\omega \frac{e^{i(\mathbf{k} \cdot \mathbf{r} + \omega t)}}{(1/\sigma_{ab} + i\omega/v_{ab})^2 + k^2}$$

$$= \frac{v_{ab}e^{-v_{ab}t/\sigma_{ab}}}{2\pi} \int_0^\infty dk \sin(kv_{ab}t) J_0(kr)$$

$$= \frac{v_{ab}e^{-v_{ab}t/\sigma_{ab}}}{2\pi} \frac{1}{\sqrt{v_{ab}^2 t^2 - r^2}} \Theta(v_{ab}t - r). \quad (30)$$

## Appendix B

Here we provide some details on the simulation strategy for equations of the form (15). By defining some auxilliary variables and applying the chain rule this can be written as four first-order (in time) PDEs. For our choice of  $\eta$ , equation (1) can be written

$$\left[\frac{1}{\alpha_{ab}\beta_{ab}}\frac{\partial^2}{\partial t^2} + \left(\frac{\alpha_{ab} + \beta_{ab}}{\alpha_{ab}\beta_{ab}}\right)\frac{\partial}{\partial t} + 1\right]u_{ab} = \psi_{ab}(t - \tau_{ab}).$$
(31)

Note that for simplicity we set  $\tau_{ab} = 0$  in our simulations. To solve an equation like (29) we let  $\psi_{ab}^{\mathbf{q}} = e^{i\mathbf{q}\cdot\mathbf{r}}\hat{\psi}_{ab}^{\mathbf{q}}$ , which converts (29) to

$$(\mathcal{A}_{ab;\epsilon_1} - \nabla^2)(\mathcal{A}_{ab;\epsilon_2} - \nabla^2)\widehat{\psi}_{ab}^{\mathbf{q}} = e^{-i\mathbf{q}\cdot\mathbf{r}}w_{ab}^0\mathcal{B}_{ab}\rho_b, \quad (32)$$

and then proceed as above. The square domains were discretised with a regular grid and the spatial deriva-

tives were approximated using finite differences. Periodic boundary conditions were used. The resulting ODEs were integrated using ode45 in Matlab with default tolerances. Figure 3 had a discretisation of  $60 \times 60$ , Fig. 4 was  $51 \times 51$ , Fig. 8 was  $20 \times 20$  and Fig. 9 used  $50 \times 50$ .

- H R Wilson and J D Cowan. A mathematical theory of the functional dynamics of cortical and thalamic nervous tissue. *Kybernetik*, 13:55–80, 1973.
- [2] S Amari. Dynamics of pattern formation in lateralinhibition type neural fields. *Biological Cybernetics*, 27:77–87, 1977.
- [3] G B Ermentrout. Neural nets as spatio-temporal pattern forming systems. Reports on Progress in Physics, 61:353– 430, 1998.
- [4] V K Jirsa. Connectivity and dynamics of neural information processing. *Neuroinformatics*, 2:183–204, 2004.
- [5] S Coombes. Waves, bumps, and patterns in neural field theories. *Biological Cybernetics*, 93:91–108, 2005.
- [6] D J Pinto and G B Ermentrout. Spatially structured activity in synaptically coupled neuronal networks: I. Travelling fronts and pulses. SIAM Journal on Applied Mathematics, 62:206–225, 2001.
- [7] S Coombes, G J Lord, and M R Owen. Waves and bumps in neuronal networks with axo-dendritic synaptic interactions. *Physica D*, 178:219–241, 2003.
- [8] A Hutt, M Bestehorn, and T Wennekers. Pattern formation in intracortical neuronal fields. *Network*, 14:351–368, 2003.
- [9] A Hutt. Effects of nonlocal feedback on traveling fronts in neural fields subject to transmission delay. *Physical Review E*, 70:052902, 2004.
- [10] C R Laing and S Coombes. The importance of different timings of excitatory and inhibitory pathways in neural field models. *Network*, 17:151–172, 2006.
- [11] P L Nunez. The brain wave equation: a model for the EEG. *Mathematical Biosciences*, 21:279–297, 1974.
- [12] D T J Liley, P J Cadusch, and M P Dafilis. A spatially continuous mean field theory of electrocortical activity. *Network*, 13:67–113, 2002.
- [13] V K Jirsa and H Haken. Field theory of electromagnetic brain activity. *Physical Review Letters*, 77:960–963, 1996.
- [14] C R Laing and W C Troy. PDE methods for nonlocal models. SIAM Journal on Applied Dynamical Systems, 2:487–516, 2003.
- [15] M L Steyn-Ross, D A Steyn-Ross, J W Sleigh, and D T J Liley. Theoretical electroencephalogram stationary spectrum for a white-noise-driven cortex: Evidence for a general anesthetic-induced phase transition. *Physical Review* E, 60:7299-7311, 1999.
- [16] P A Robinson, C J Rennie, J J Wright, H Bahramali, E Gordon, and D l Rowe. Prediction of electroencephalographic spectra from neurophysiology. *Physical Review* E, 63:021903, 2001.
- [17] I Bojak and D T J Liley. Modeling the effects of an esthesia on the electroencephalogram. *Physical Review E*,

- 71:041902, 2005.
- [18] A Hutt. Examination of a neuronal field equation based on a MEG-experiment in humans. Diploma Thesis at Institute for Theoretical Physics and Synergetics, University of Stuttgart, 1997.
- [19] S E Folias and P C Bressloff. Breathing pulses in an excitatory neural network. SIAM Journal on Applied Dynamical Systems, 3:378–407, 2004.
- [20] P C Bressloff. Spatially periodic modulation of cortical patterns by long-range horizontal connections. *Physica* D, 185:131–157, 2003.
- [21] P A Robinson. Patchy propagator, brain dynamics, and the generation of spatially structured gamma oscillations. *Physical Review E*, 73:041904, 2006.
- [22] P L Nunez. Neocortical Dynamics and Human EEG Rhythms. Oxford University Press, 1995.
- [23] P L Nunez and R Srinivasan. *Electric Fields of the Brain*. Oxford University Press, 2nd edition, 2006.
- [24] N A Venkov, S Coombes, and P C Matthews. Dynamic instabilities in scalar neural field equations with spacedependent delays. *Physica D*, 232:1–15, 2007.
- [25] G Dangelmayr and M Wegelin. Pattern Formation in Continuous and Coupled Systems: A Survey Volume, volume 115 of IMA Volumes in Mathematics & Its Applications, chapter On Primary and Secondary Hopf Bifurcations in Anisotropic Systems, pages 33–48. Springer-Verlag, New York, 1999.
- [26] C R Laing. Spiral waves in nonlocal equations. SIAM Journal on Applied Dynamical Systems, 4:588–606, 2005.
- [27] M R Owen, C R Laing, and S Coombes. Bumps and rings in a two-dimensional neural field: splitting and rotational instabilities. *submitted*, 2007.
- [28] F M Atay and A Hutt. Neural fields with distributed transmission speeds and long-range feedback delay. SIAM Journal Applied Dynamical Systems, 5:670– 698, 2006.
- [29] A Hutt and F M Atay. Effects of distributed transmission speeds on propagating activity in neural populations. *Physical Review E*, 73:021906, 2006.
- [30] A Hutt and F M Atay. Spontaneous and evoked activity in extended neural populations with gamma-distributed spatial interactions and transmission delay. *Chaos, Solitons & Fractals*, 32:547–560, 2007.
- [31] V K Jirsa and J A S Kelso. Spatiotemporal pattern formation in neural systems with heterogeneous connection topologies. *Physical Review E*, 62:8462–8465, 2000.
- [32] P A Robinson, C J Rennie, and J J Wright. Propagation and stability of waves of electrical activity in the cerebral cortex. *Physical Review E*, 56:826–840, 1997.